

From Bench to Brain

In Situ Tissue Engineering for Brain Aneurysms



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SIMI 2016 – 25th Anniversary; Buenos Aires



Disclosures

- Research Grants

(last 12 months):

- NINDS, NIBIB, NIA, NCI
- Philips Healthcare
- MicroVention/Terumo
- Stryker Neurovascular
- Codman Neurovascular
- eV3 Neurovascular / Covidien
- InNeuroCo Inc
- Blockade Medical
- CereVasc LLC
- Genuity
- Cook Medical
- Neuronal Protection Systems LLC
- Spineology Inc
- Silk Road
- Wyss Institute
- Neuravi

- Consulting

(fee-per-hour, last 12 months):

- Stryker Neurovascular
- Codman Neurovascular

- Investment (Stocks)

- InNeuroCo Inc

Patient-Specific Hemodynamic Analysis and Treatment Efficacy (Flow Diversion)

Flow Mechanics

Flow driven by ΔP

Momentum Transfer



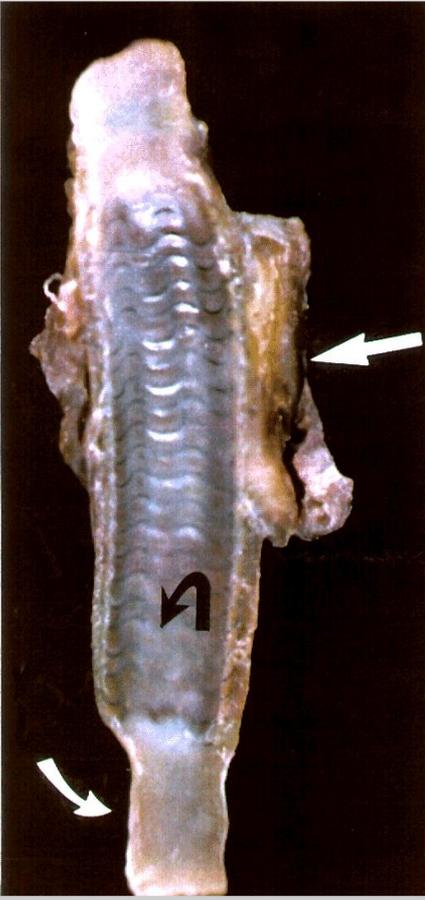
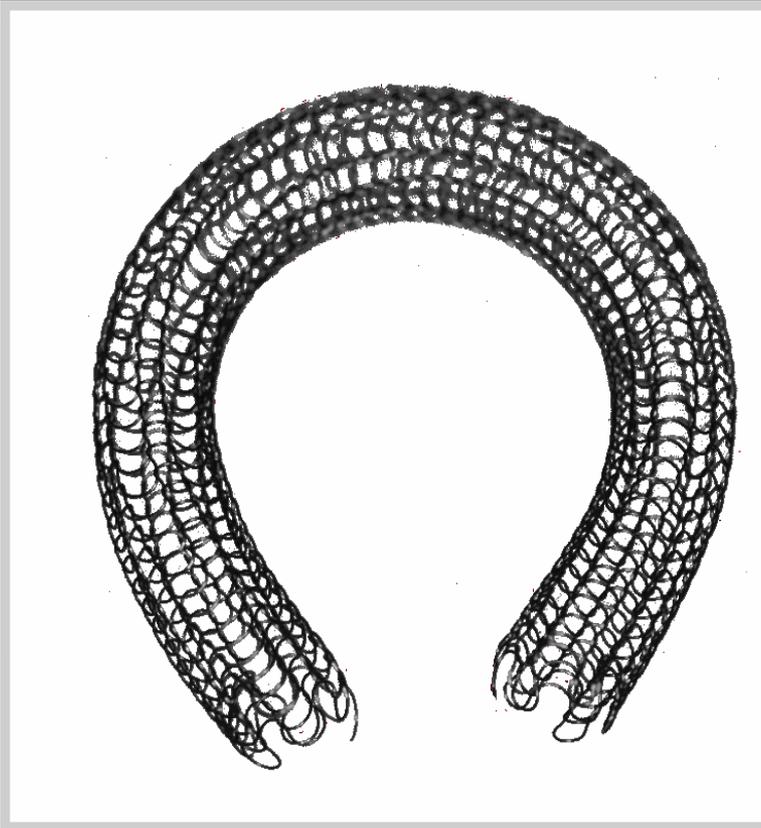
Fundamental Goal: Design technology that can disrupt momentum transfer into the aneurysm producing exclusion from the circulation without occluding perforators/ jailed vessels

In a Word(s)...

- BETTER – in situ tissue engineering

Submission Deadline 2/1/03	Project Start Date 12/1/03	Project End Date 11/30/03	Campus Medical
Principal Investigator: Baruch Barry Lieber, PhD		Co-Principal Investigator: Ajay Kumar Wakhloo, MD, PhD	
Soc. Sec. #: 250-35-6784	Phone No.: 305-284-6476	Soc. Sec. #: 600-25-0062	Phone No.: 305-585-8186
School: College of Engineering	Home Department: Biomedical Engineering	School: Medicine	Home Department: Radiology
Accounting Department (if different from Radiology)			
Project Title: Flow Divertors to Cure Cerebral Aneurysms			
Sponsoring Agency (if a private foundation, see footnote below) National Institutes of Health		Person assisting with budget Name: Roberta Turner/Dagmar Schnau RT 8-2445 Dagmar 585-817	
Joint Proposal: % distribution between Depts/Div's: Radiology 50% Biomedical Engineering 50%			
Type of Project: <input checked="" type="checkbox"/> Research <input type="checkbox"/> Clinical Trial <input type="checkbox"/> Training <input type="checkbox"/> Construction <input type="checkbox"/> Other _____			
Type of Proposal: <input type="checkbox"/> New <input checked="" type="checkbox"/> Revision <input type="checkbox"/> Supplemental <input type="checkbox"/> Competitive Renewal <input type="checkbox"/> Non-Competitive Renewal			
Budget Summary (details attached)			
1st Year	2nd Year	3rd Year	4th Year

The Observation

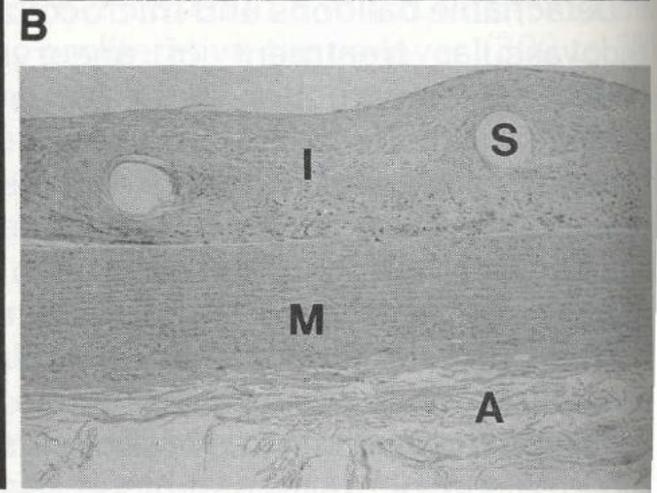
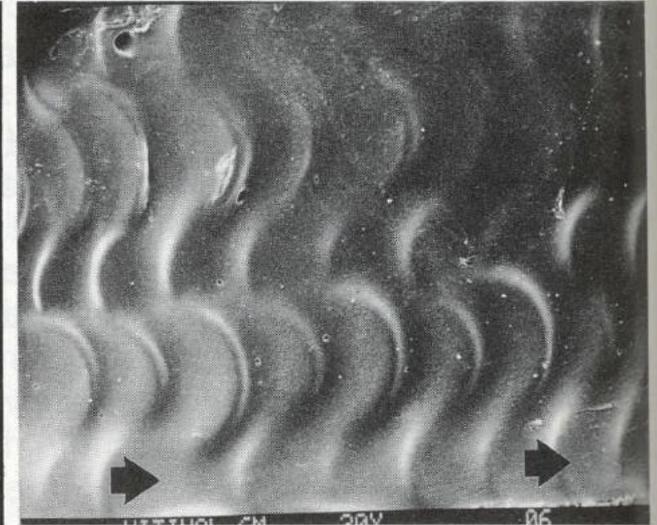
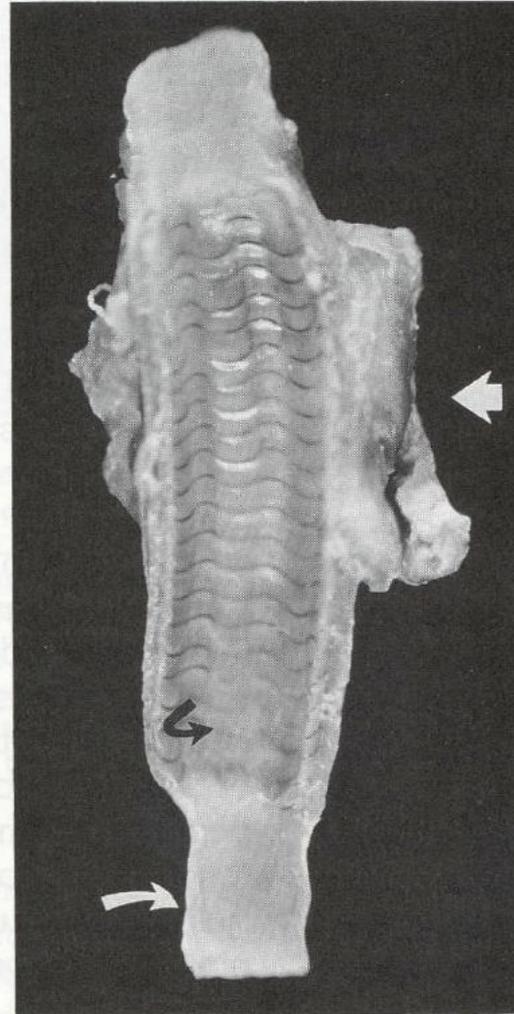


Step 2: Tissue Engineering

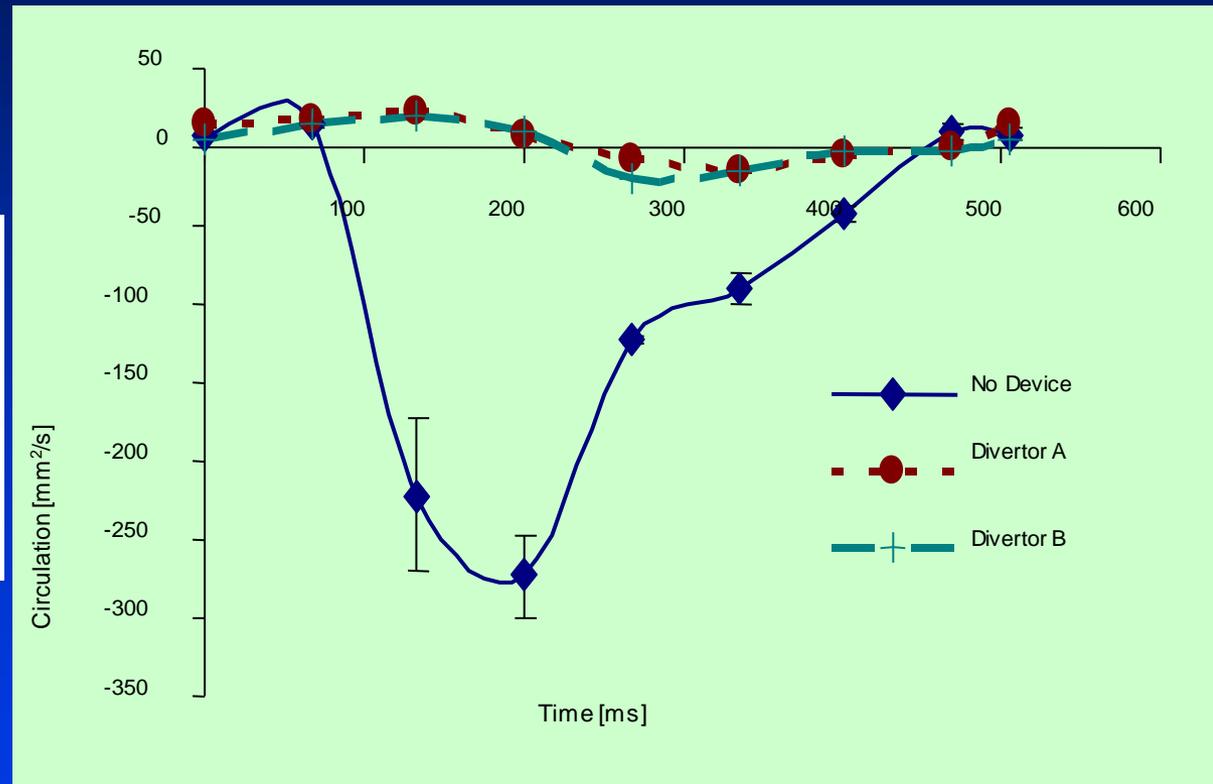
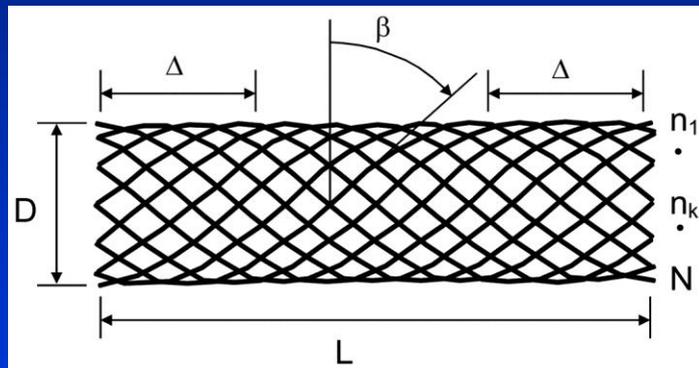
Fig. 7. Longitudinal section of a formaldehyde-fixated common carotid artery with thrombosed and organized lateral aneurysm (*short arrow*). The vessel (original diameter approximately 3.8 mm) was harvested 6 months after implantation of a heat-treated self-expanding nitinol stent (5-mm diameter in fully expanded state). A thin intimal fibrocellular tissue is covering the struts (*curved black arrow*). There is a markedly thickened vessel wall in the stented portion including the ostium of the aneurysm because of intimal proliferation. (Note the artificial reduction of the nonstented vessel segment after resection and fixation compared with the treated rigid part, *curved white arrow*).

B, Scanning electron photomicrograph of a carotid artery harvested 6 months after nitinol stent placement demonstrates the flow-induced macroscopic architecture of the neointima (original magnification $\times 20$).

C, Transverse section of a common carotid artery 6 months after implantation of a nitinol stent (hematoxylin and eosin stain, original magnification $\times 25$). I indicates intima; M, media; A, adventitia; S, empty space corresponding to stent filaments. Thickness of intima covering the filaments is approximately $80\ \mu\text{m}$ and between the



Mean Circulation: Function of FD Design



Sadasivan and Lieber, Stroke 2010

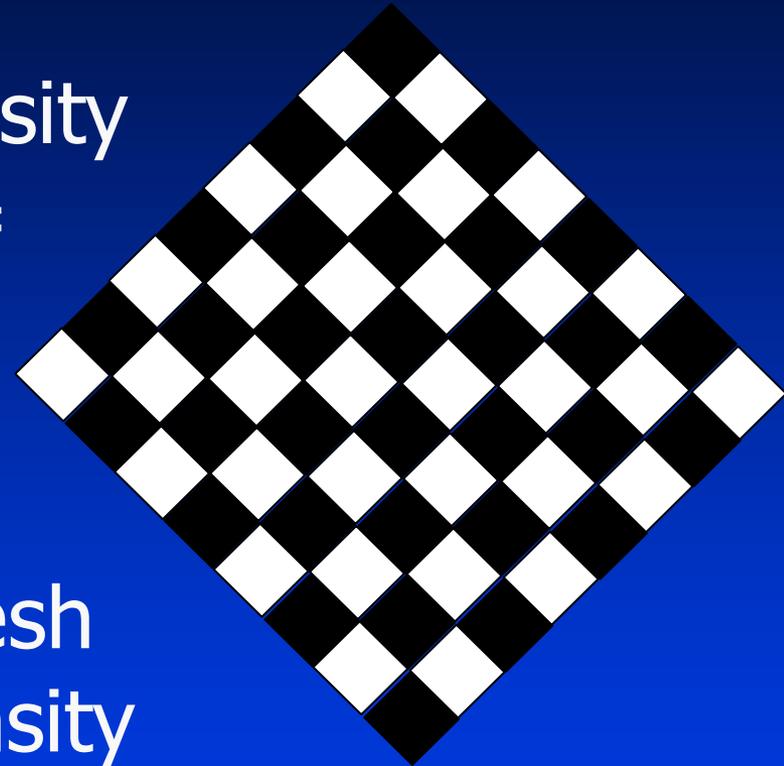
Seong, Lieber, Wakhloo. J Biomech Eng 2007

Porosity and Mesh Density



Porosity

=

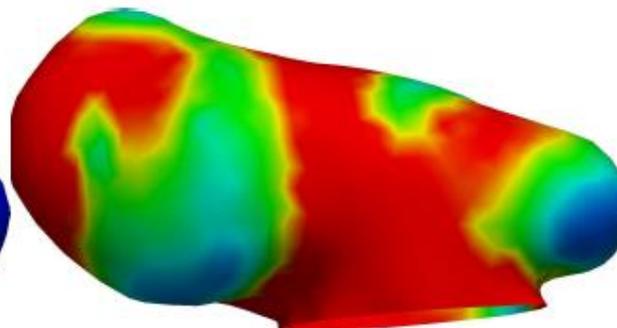
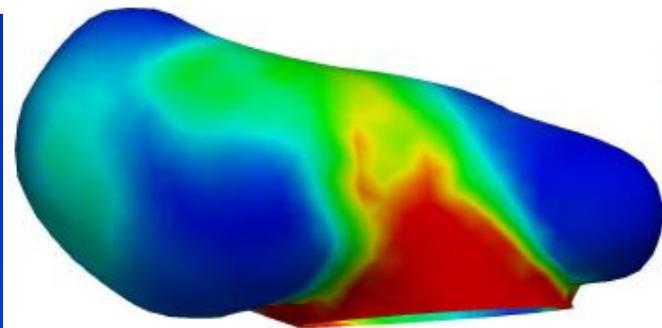
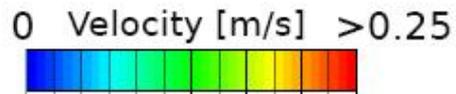
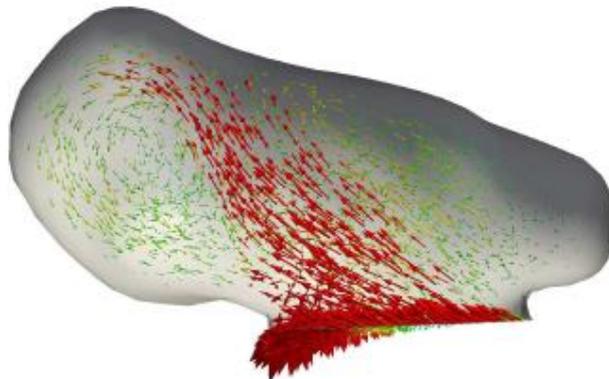
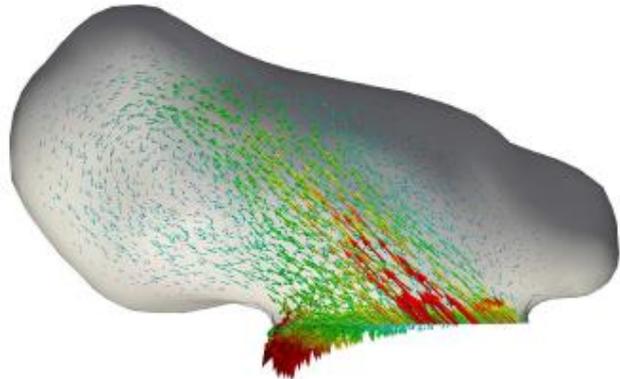
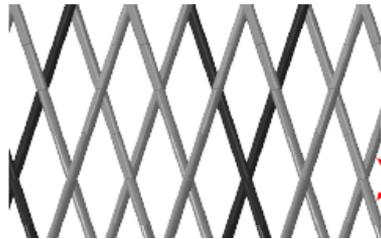


Mesh
Density

<

50% Metal Coverage
2 pores per diamond

50% Metal Coverage
32 pores per diamond



Courtesy of
Matthieu De Beule,
FEops



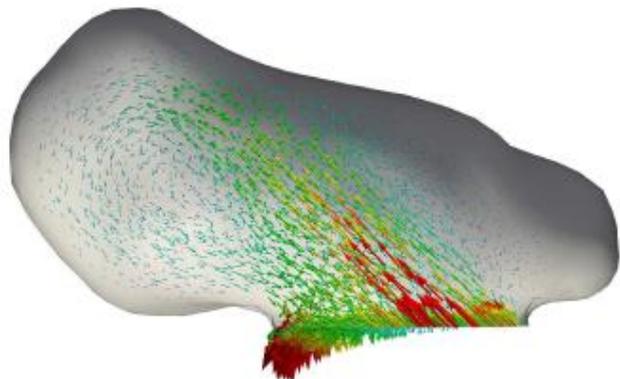
Braid angle
 109°



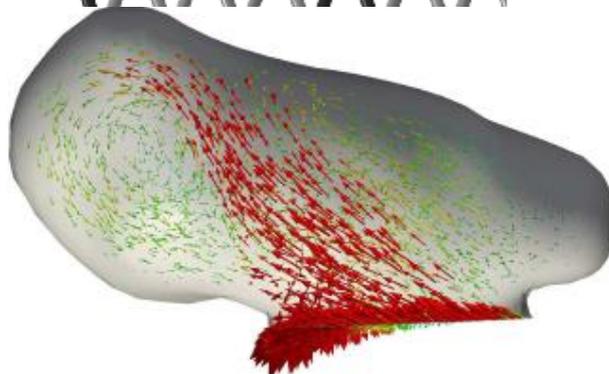
Braid angle
 150°



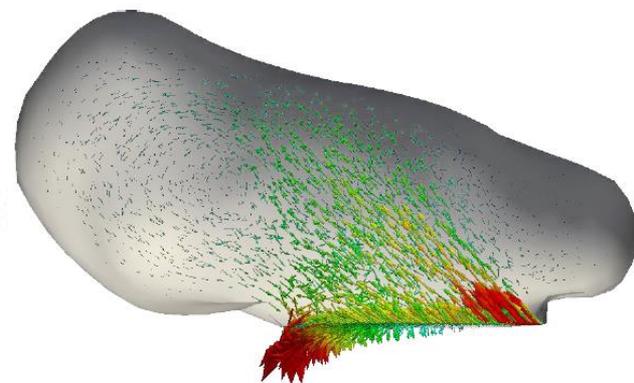
Braid angle
 115°



96 wires



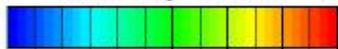
48 wires



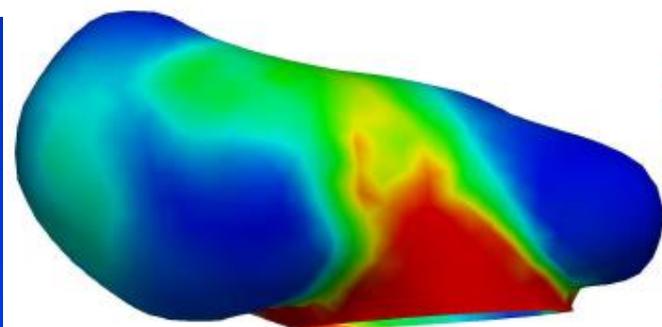
Velocity vectors

0 Velocity [m/s] >0.25

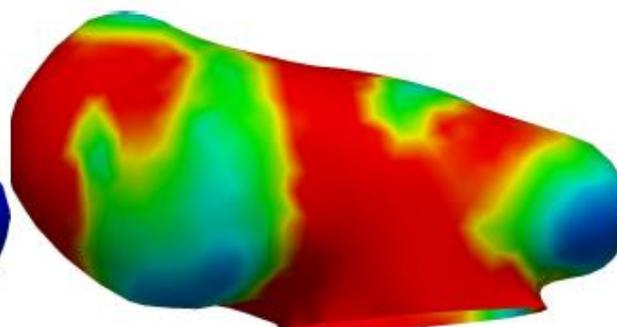
0 Velocity [m/s] >0.25



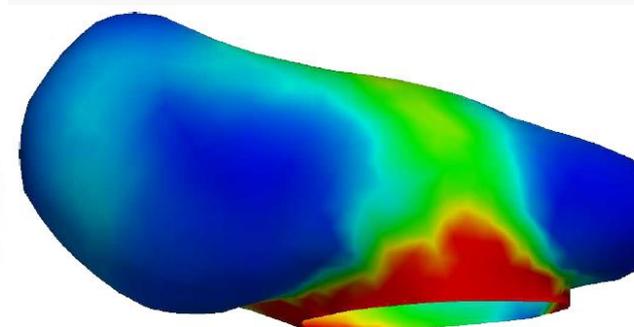
72 wires



96 wires

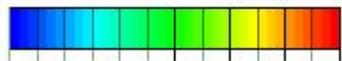


48 wires



0 WSS [Pa] >2

0 WSS [Pa] >2



72 wires

Courtesy of
Matthieu De Beule,
FEops

Mean Circulation: Function of FD Design

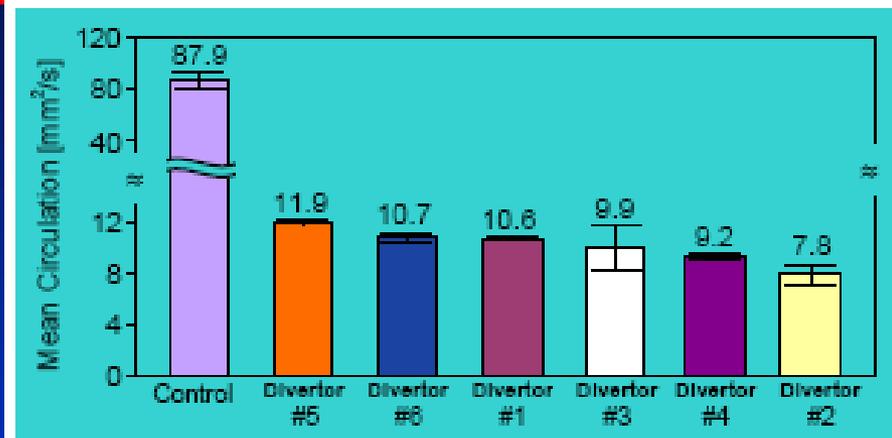
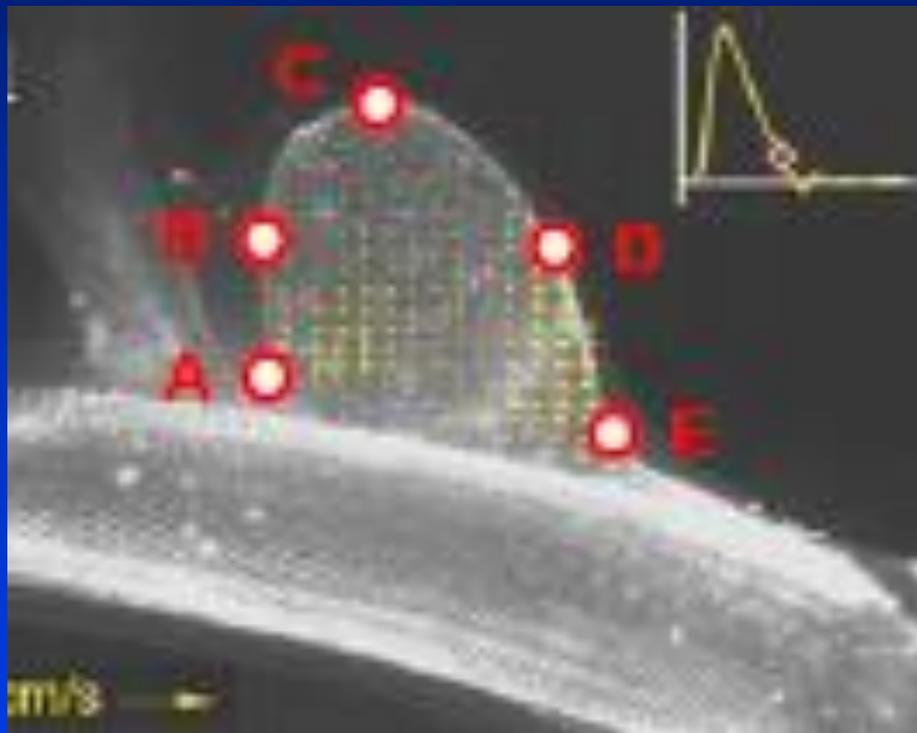


Figure 3. Mean hydrodynamic circulation inside the aneurysm before/after implantation of flow divertors.

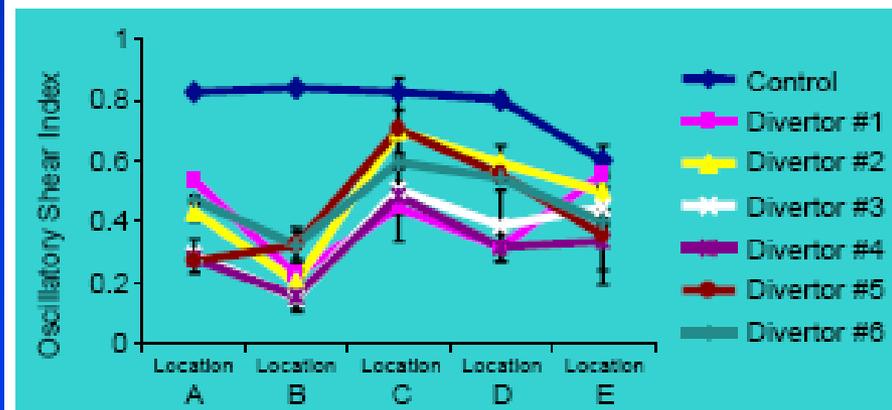


Figure 4. Oscillatory shear index (OSI) at five locations along the wall of the aneurysm sac for all divertors. Error bars denote standard error of mean (n=3).

Fate of Perforators/ Jailed Arteries

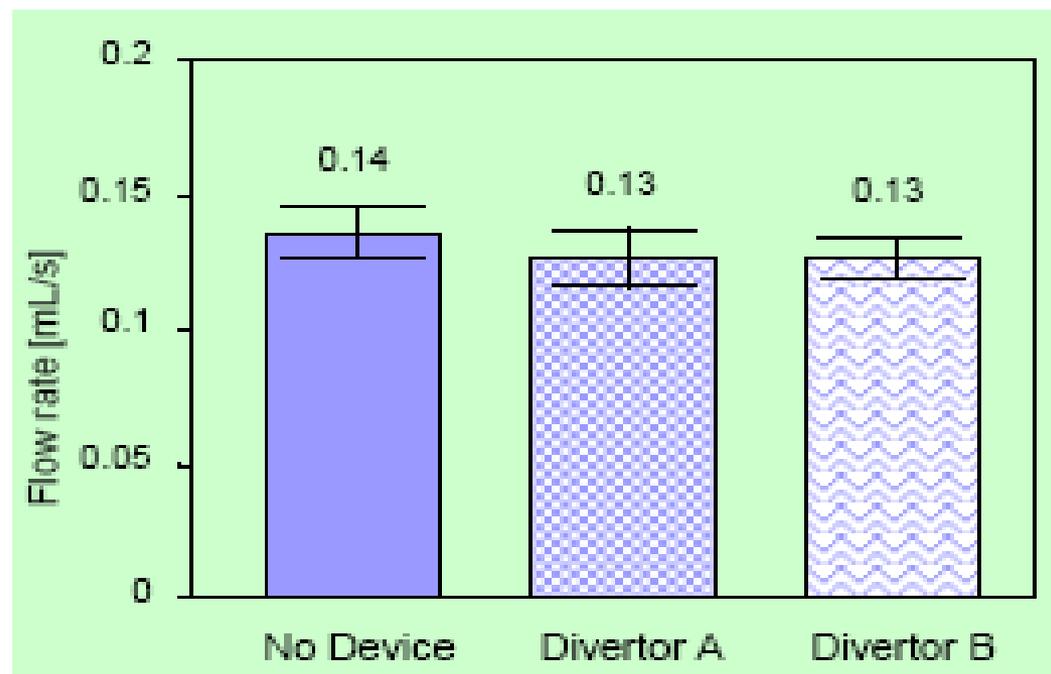
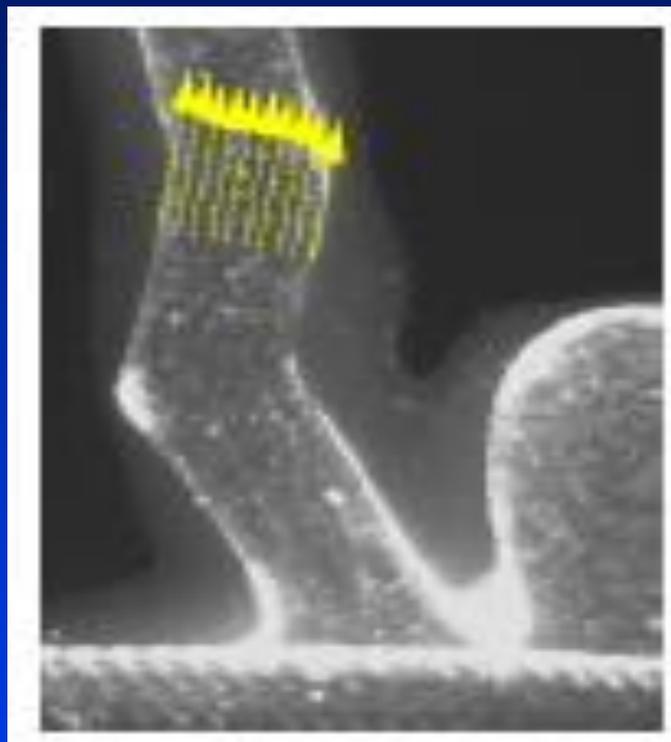
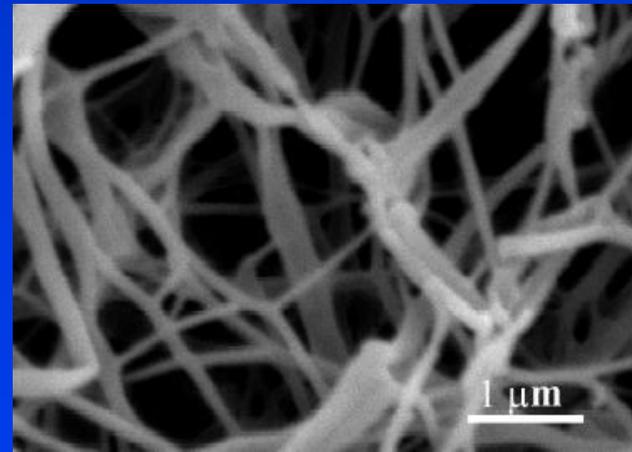
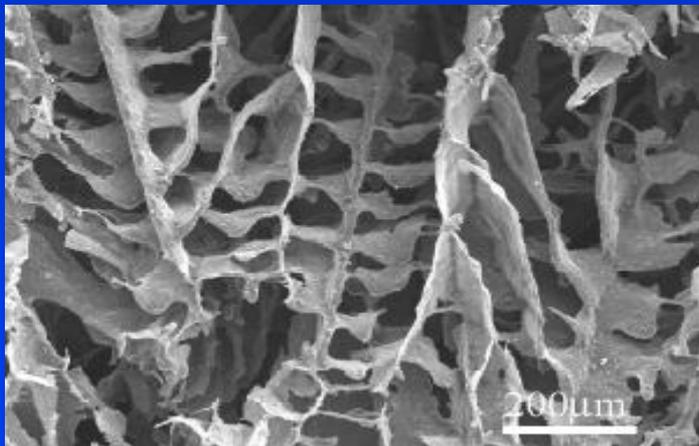


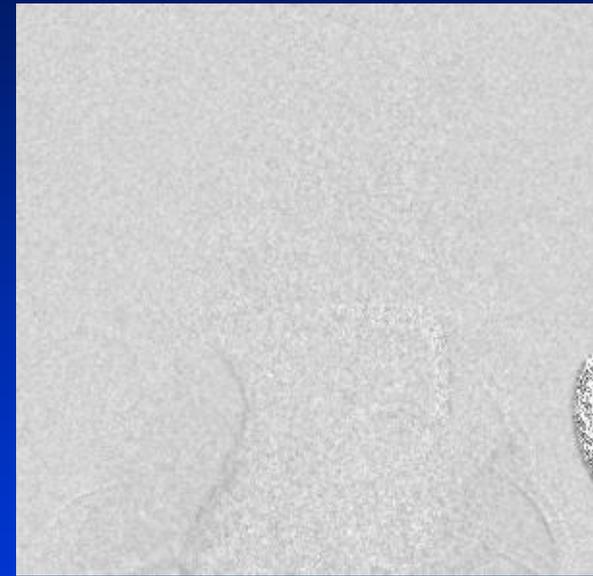
Figure 11: Mean flow rate in the vertebral artery before and after implantation of flow divertors.

Do Engineering Models Translate to In Vivo

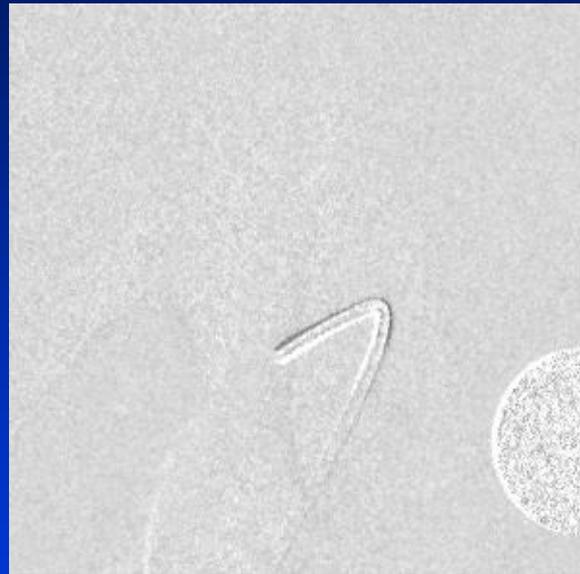
- Hypothesis: FDs with high/uniform pore density accelerate cell growth (formation of the neointima).
- Goal: to demonstrate formation of the basement membrane and subsequent endothelialization rates after FD implant



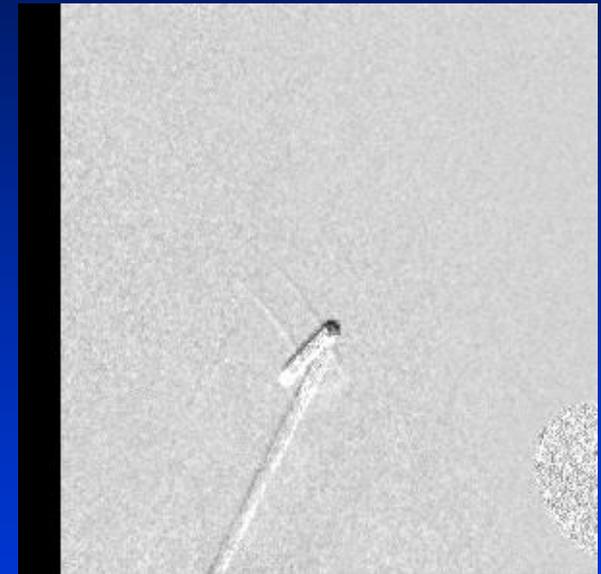
Rabbit Aneurysm Model



Pre

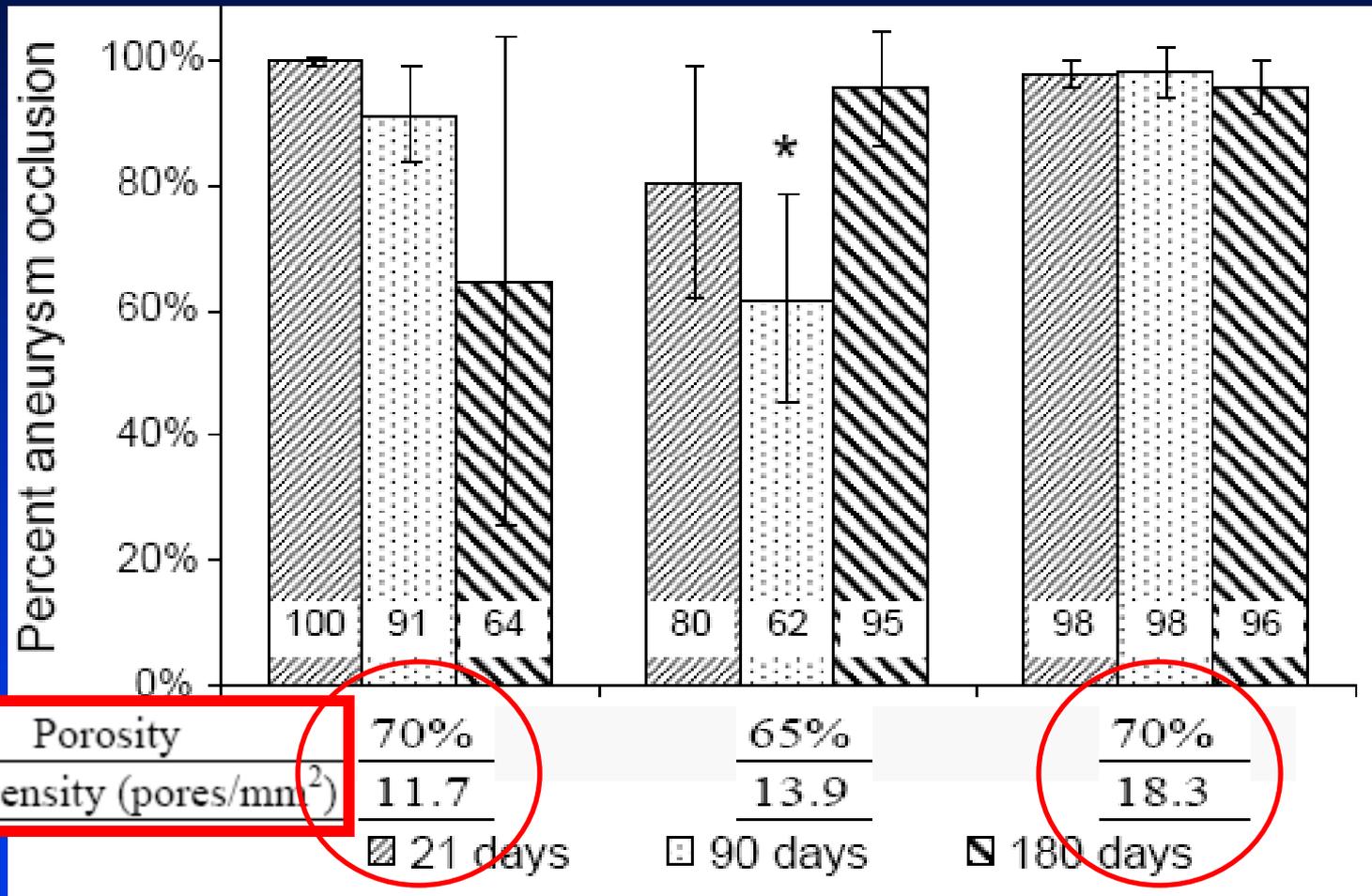


Post



FU – 1 wk

Angiographic Aneurysm Occlusion at Different Time Points

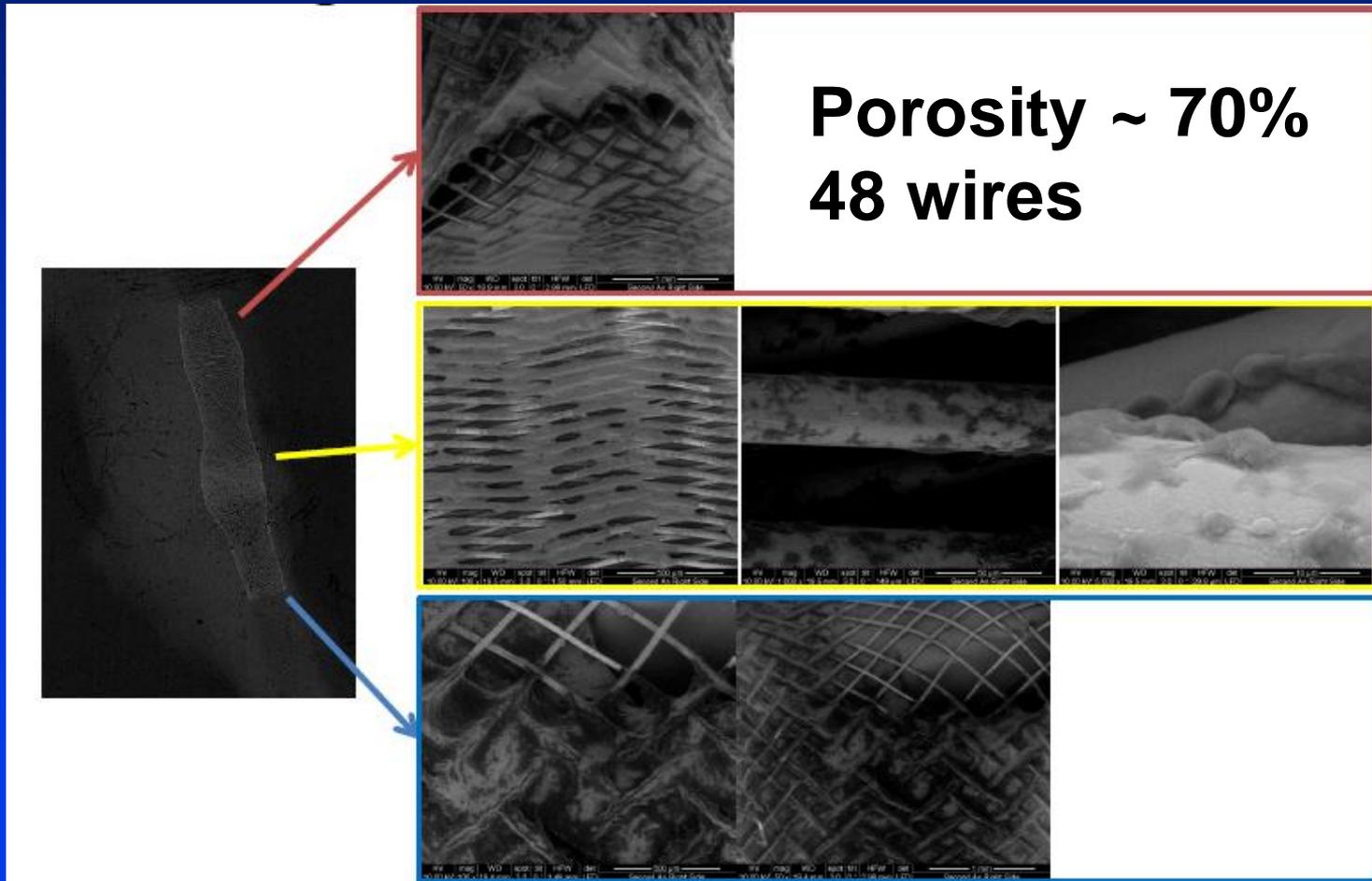


Tissue Engineering: A Function of FD Design?

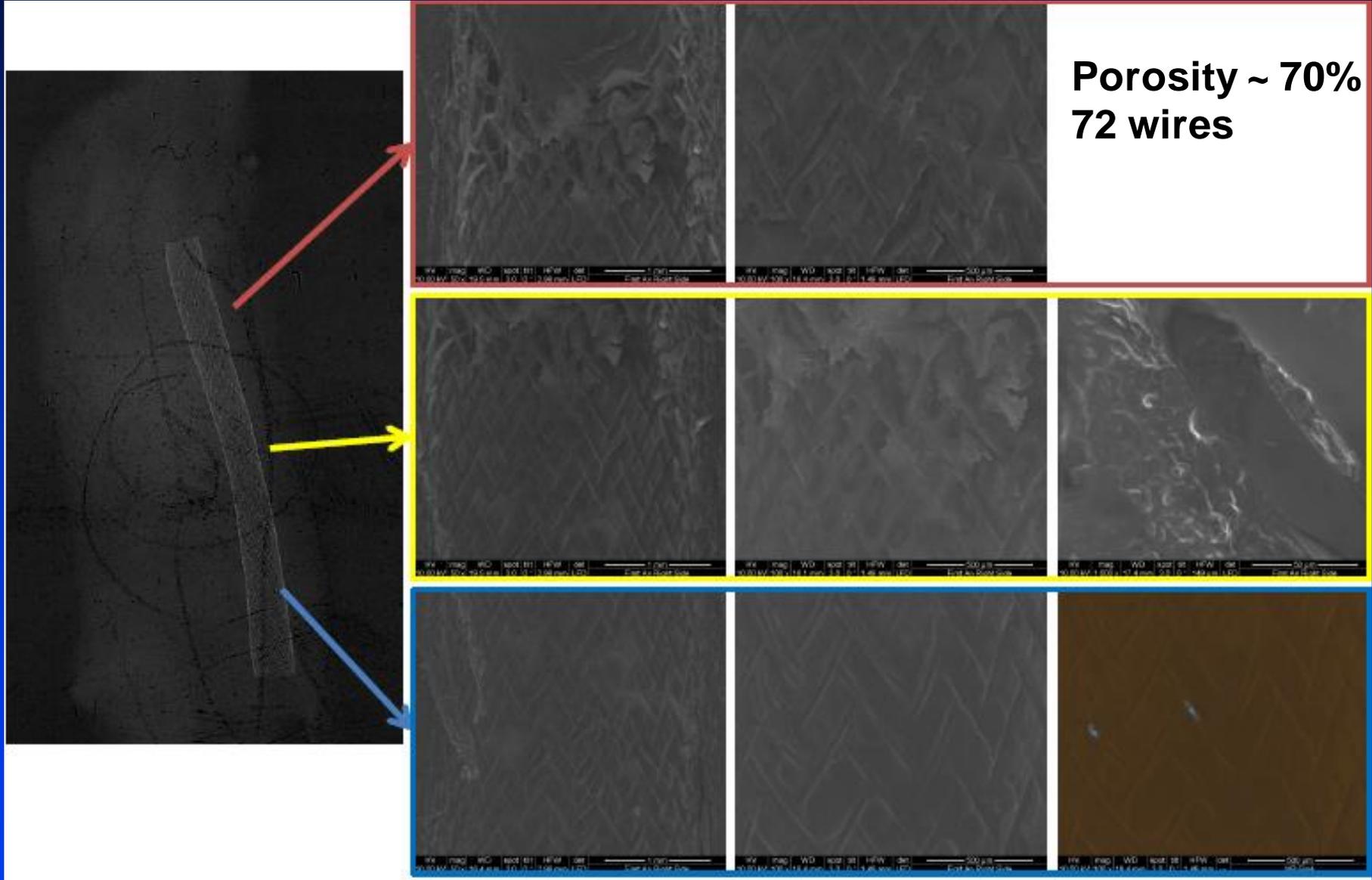


In Situ Tissue Engineering

- Canine, side-wall aneurysm – **7 days** post FD implant



In Situ Tissue Engineering



In Situ Tissue Engineering

- **The objective of this study:**
 - to demonstrate formation of the basement membrane and subsequent endothelialization rates after flow diverter stent implant

Methods

Rabbit Elastase Induced Aneurysm Model

- 24 extracranial (innominate artery) aneurysm
 - **Efficacy:**
FD endothelial coverage – histology, SEM
aneurysm occlusion rate – DSA, MR
 - **Safety (complications)**
local: FD occlusion, stenosis

- 2 different type of FD:
 - 48-Wire Device
 - 72-Wire Device

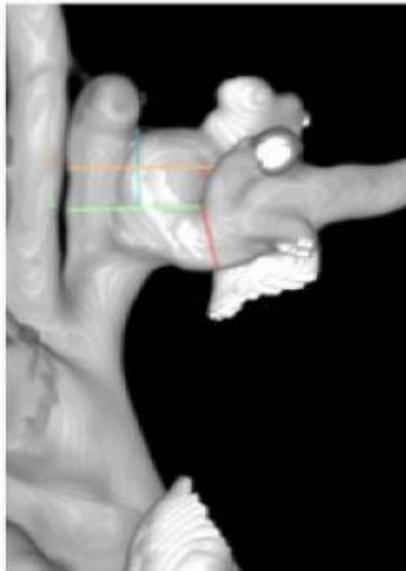
- **Periprocedural medication** (based on literature review)
 - 10mg/kg clopidogrel and
 - 1mg/kg ASA

Study Design

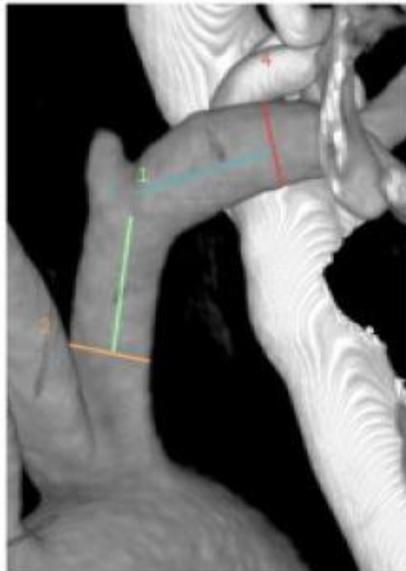
Animal grouping	Number of 72-wire FDs	Number 48-Wire FDs	FD implant procedure	Duration
Group 1	2	2	4	10 (\pm 1) days
Group 2	2	2	4	20 (\pm 2) days
Group 3	2	2	4	30 (\pm 2) days
Group 4	2	2	4	60 (\pm 2) days
Totals	8	8	16	



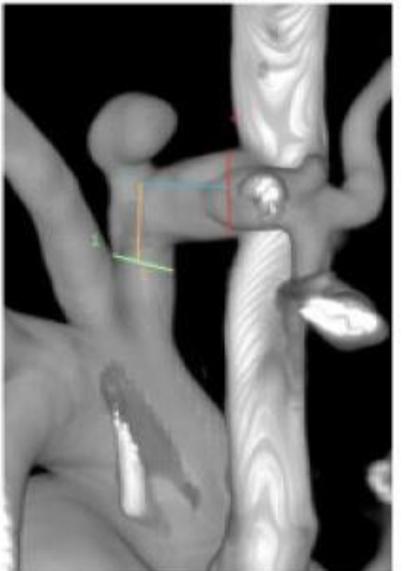
wide neck aneurysm along with distal fusiform vessel



complex, multilobular aneurysm



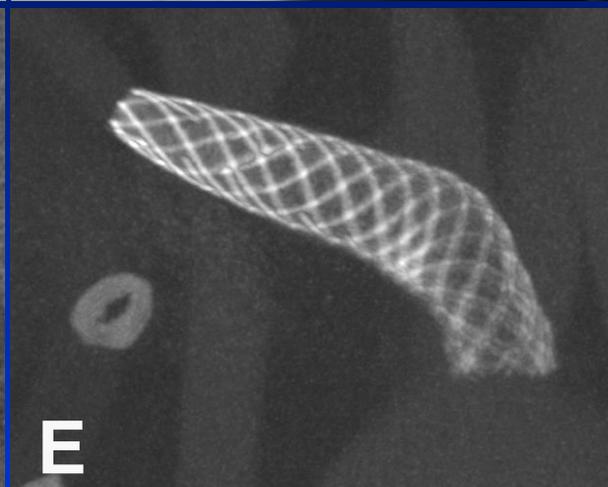
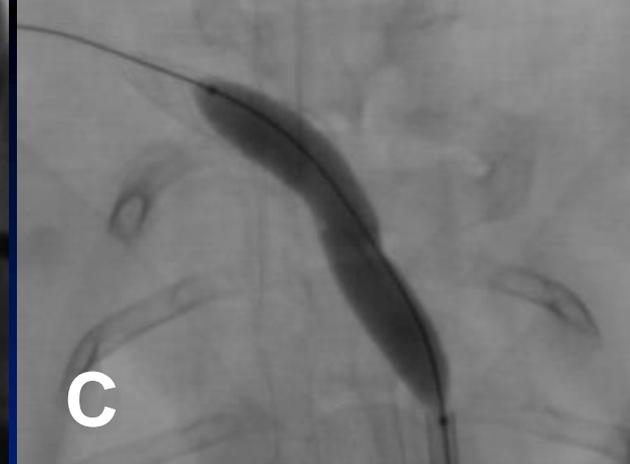
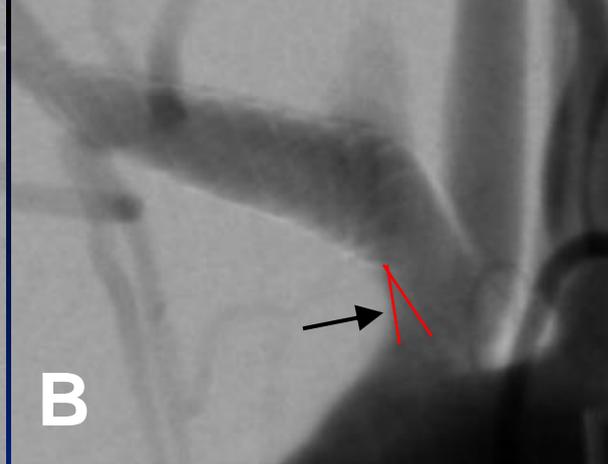
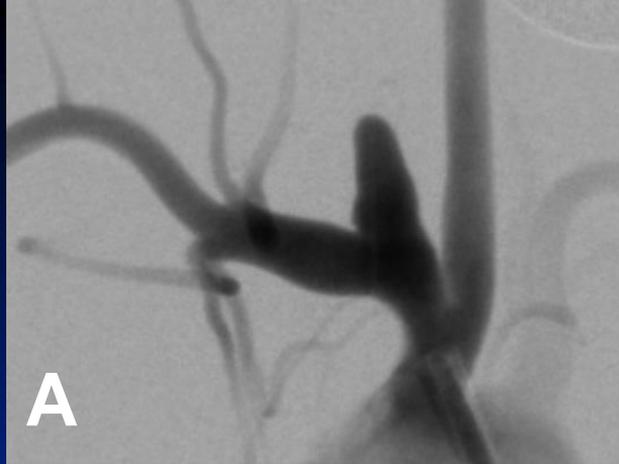
small aneurysm with wide neck and distal fusiform vessel



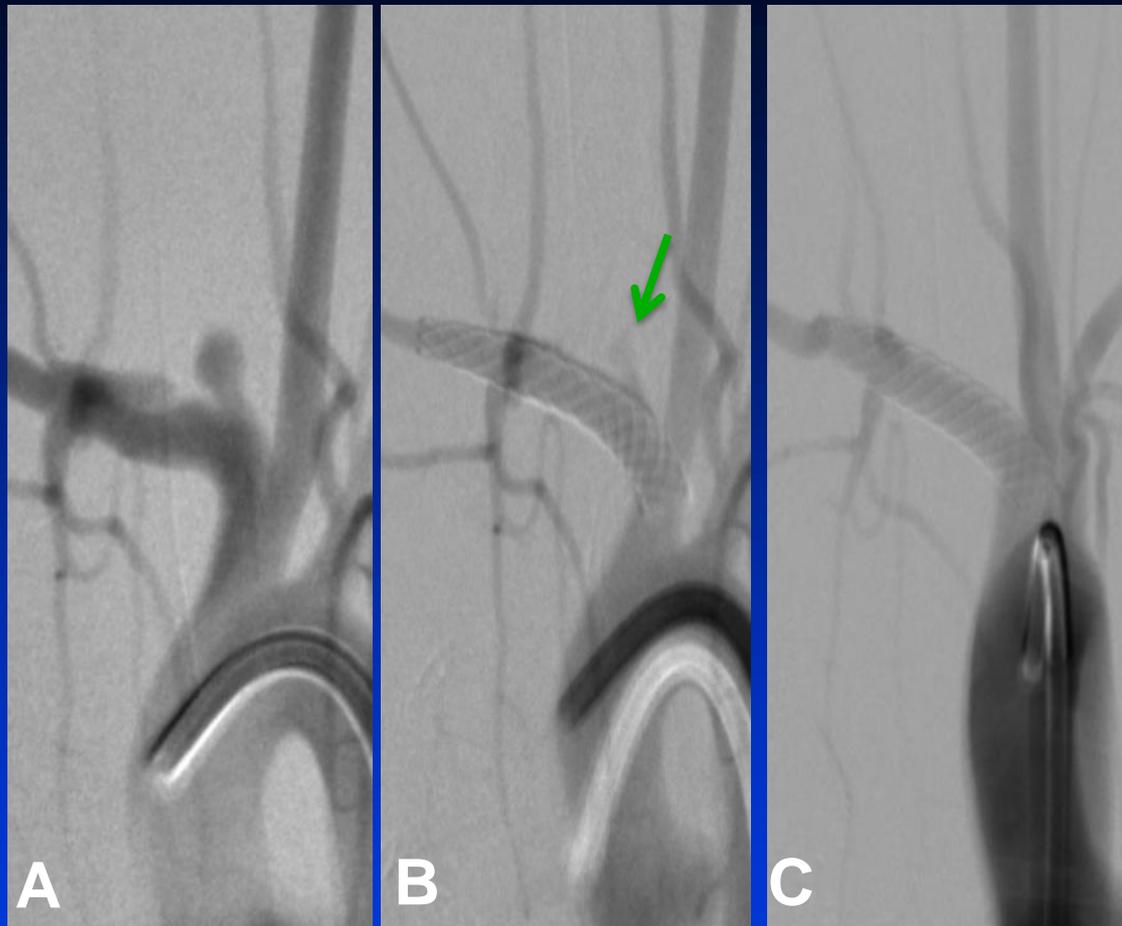
small neck aneurysm along with distal fusiform vessel

- Grouping of aneurysm was based on:
 - aneurysm morphology
 - Vessel diameter proximal and distal to the aneurysm
 - Length of proximal segment of the vessel – landing zone!!!

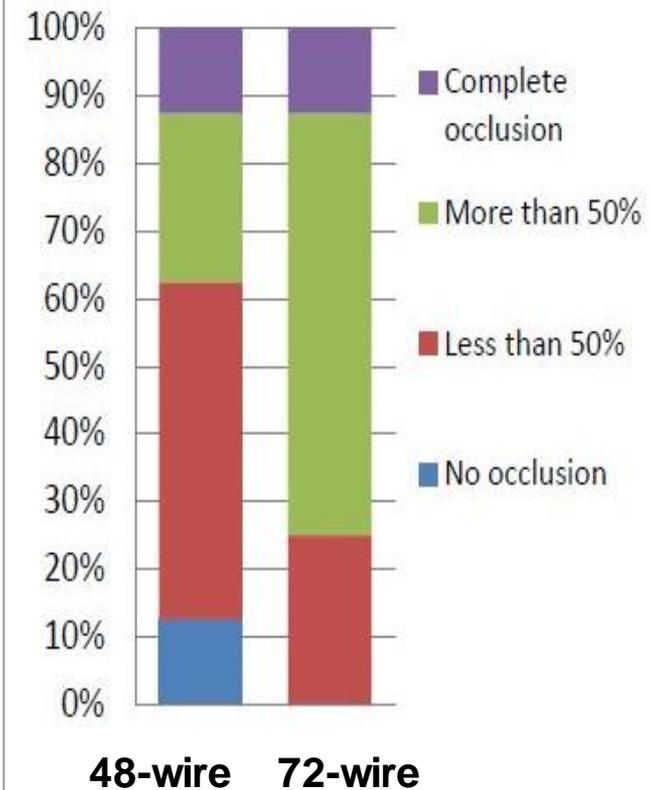
	48-wire	72-wire	p-value
<i>aneurysm height</i>	6.9 ±1.8	7.1 ±1.6	0.86
<i>aneurysm width</i>	5.5 ±2.3	5.0 ±1.9	0.64
<i>aneurysm neck</i>	5.3 ±1.9	4.6 ±1.4	0.47
<i>aspect ratio</i>	1.4 ±0.5	1.6 ±0.4	0.42
<i>parent vessel diameter 5mm distal the aneurysm</i>	4.6 ±1.0	4.4 ±0.6	0.64



- A.) Pre-procedural DSA, frontal view
- B.) Post-implant angiography, FD is not apposed at the proximal site; arrow points to the site
- C.) angioplasty
- D-E.) VasoCT, distal end of FD slightly compressed (deployed into a 2.5mm vessel), part bad apposition proximally
- F.) after 2 attempt of angioplasty DSA showed improved apposition (arrow-head)



Aneurysm occlusion rate in two compared FD groups



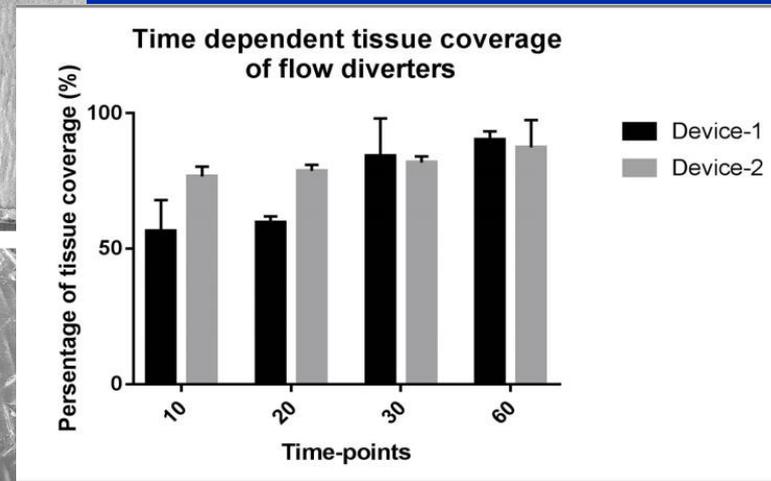
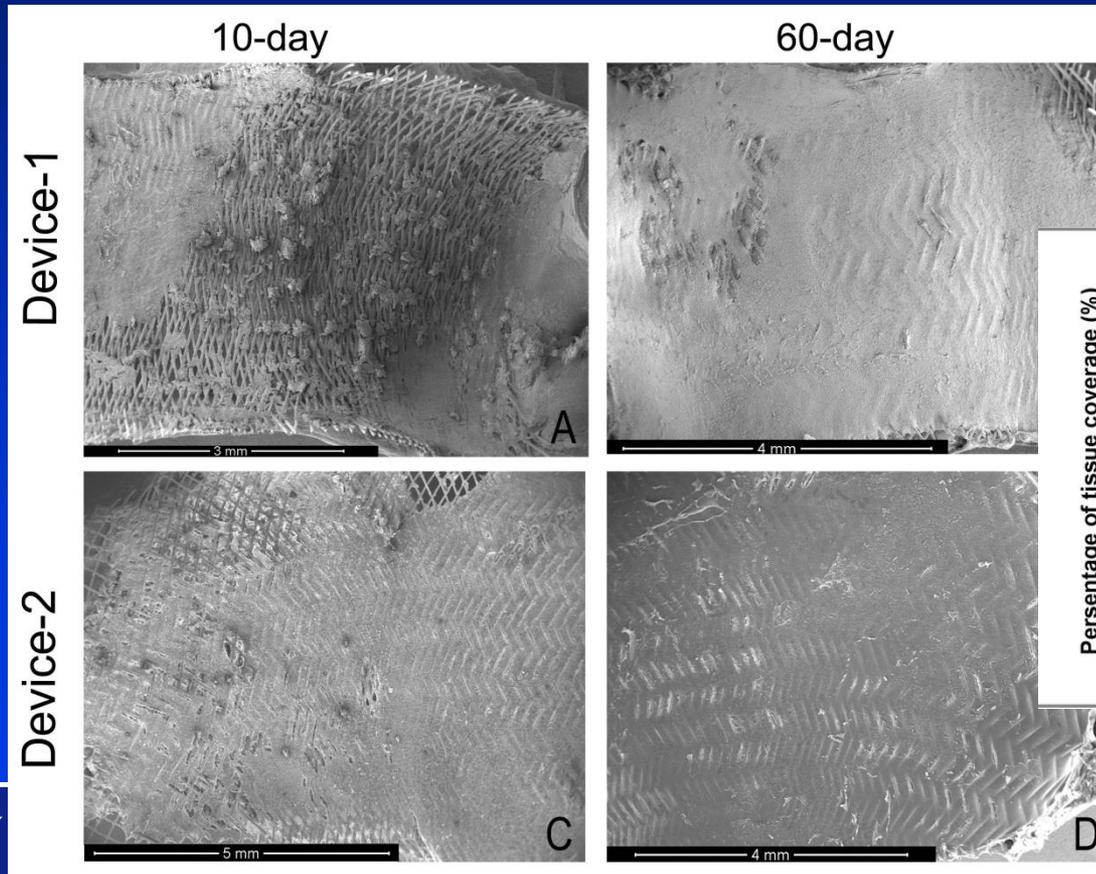
A.) DSA prior FD implant shows a small neck aneurysm with a distally dilated parent-vessel

B.) After NEG implant, some contrast inflow is still present on DSA (arrow),

C.) 30 days follow up DSA indicates complete aneurysm occlusion.

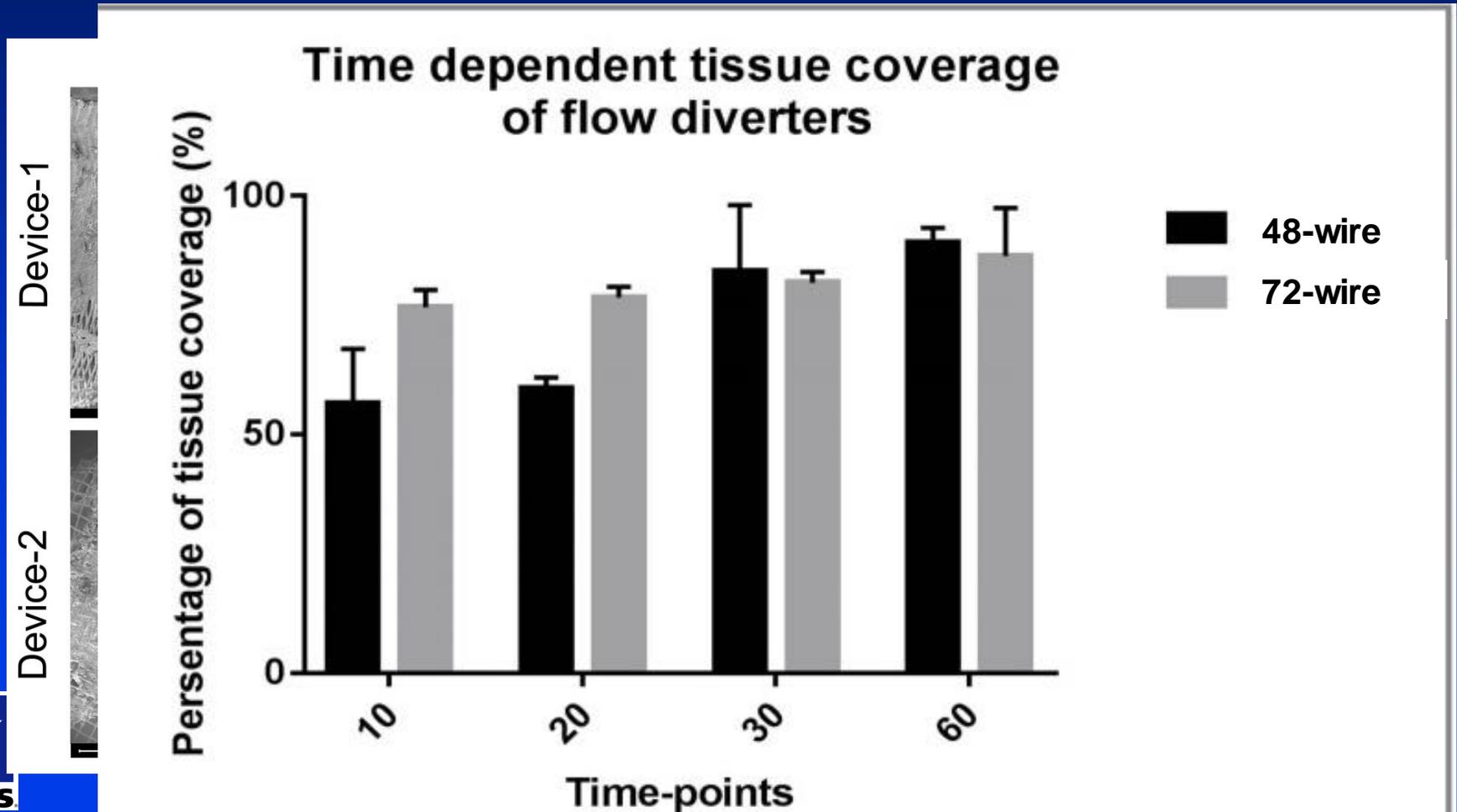
Basement Membrane

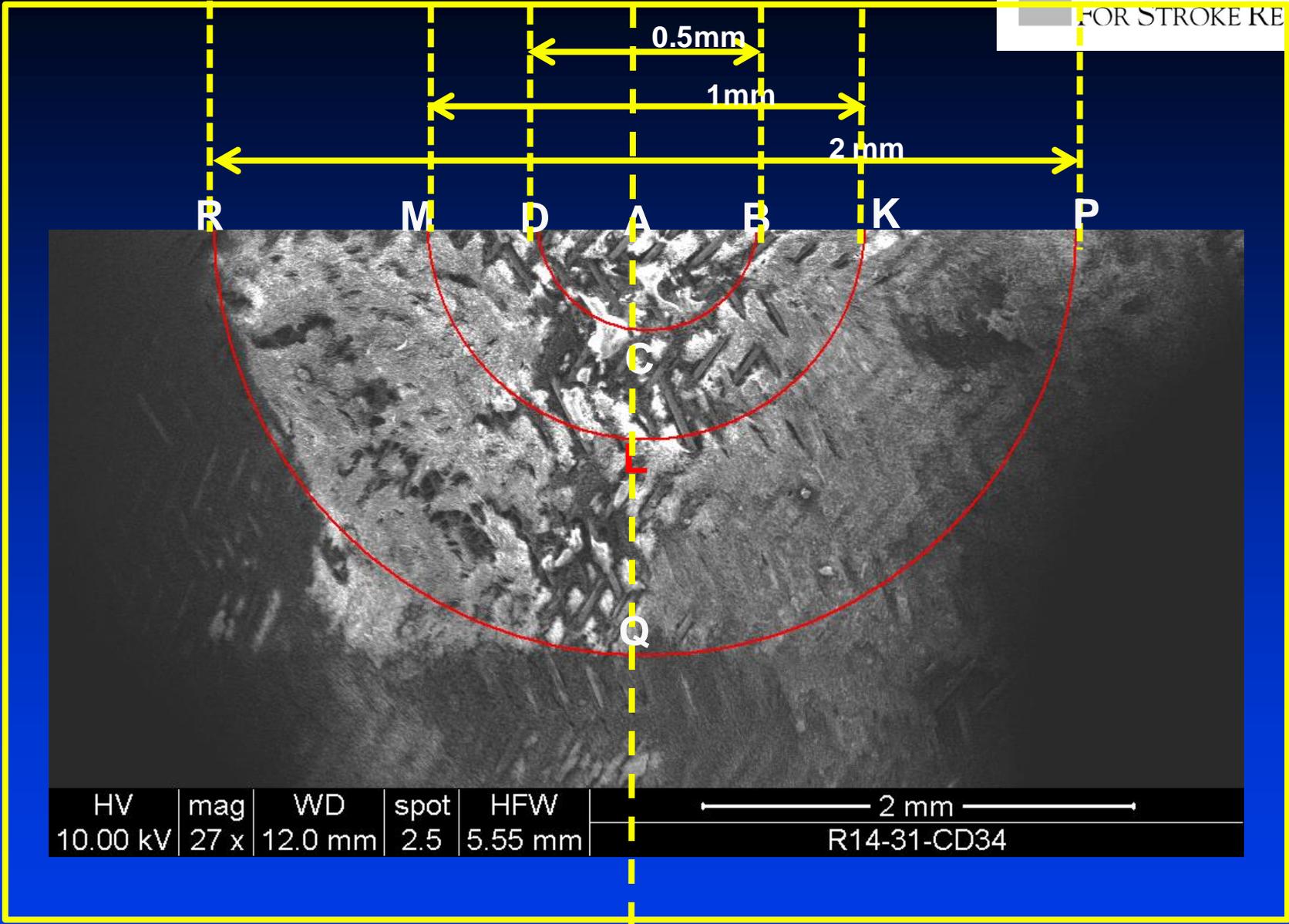
- Important first step, forms substrate for endothelialization



Basement Membrane

- Important first step, forms substrate for endothelialization





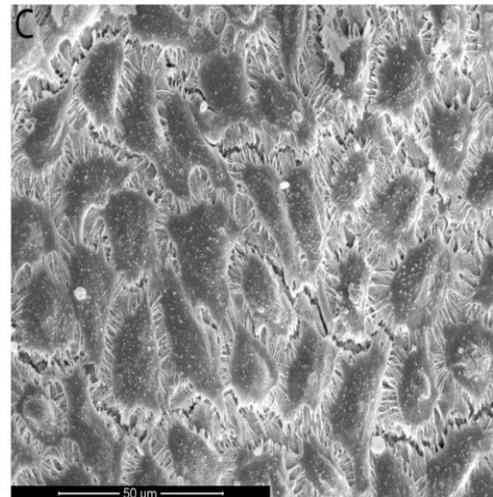
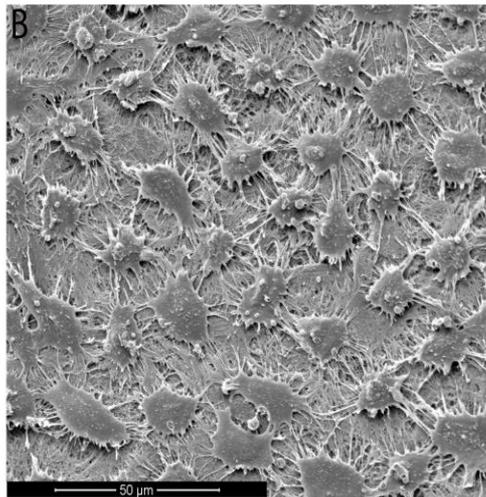
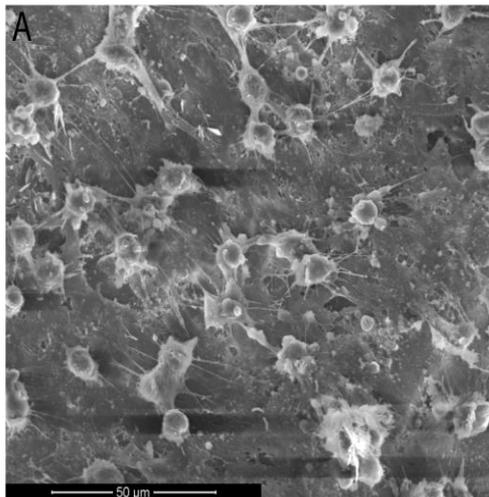
HV	mag	WD	spot	HFW
10.00 kV	27 x	12.0 mm	2.5	5.55 mm

2 mm
R14-31-CD34

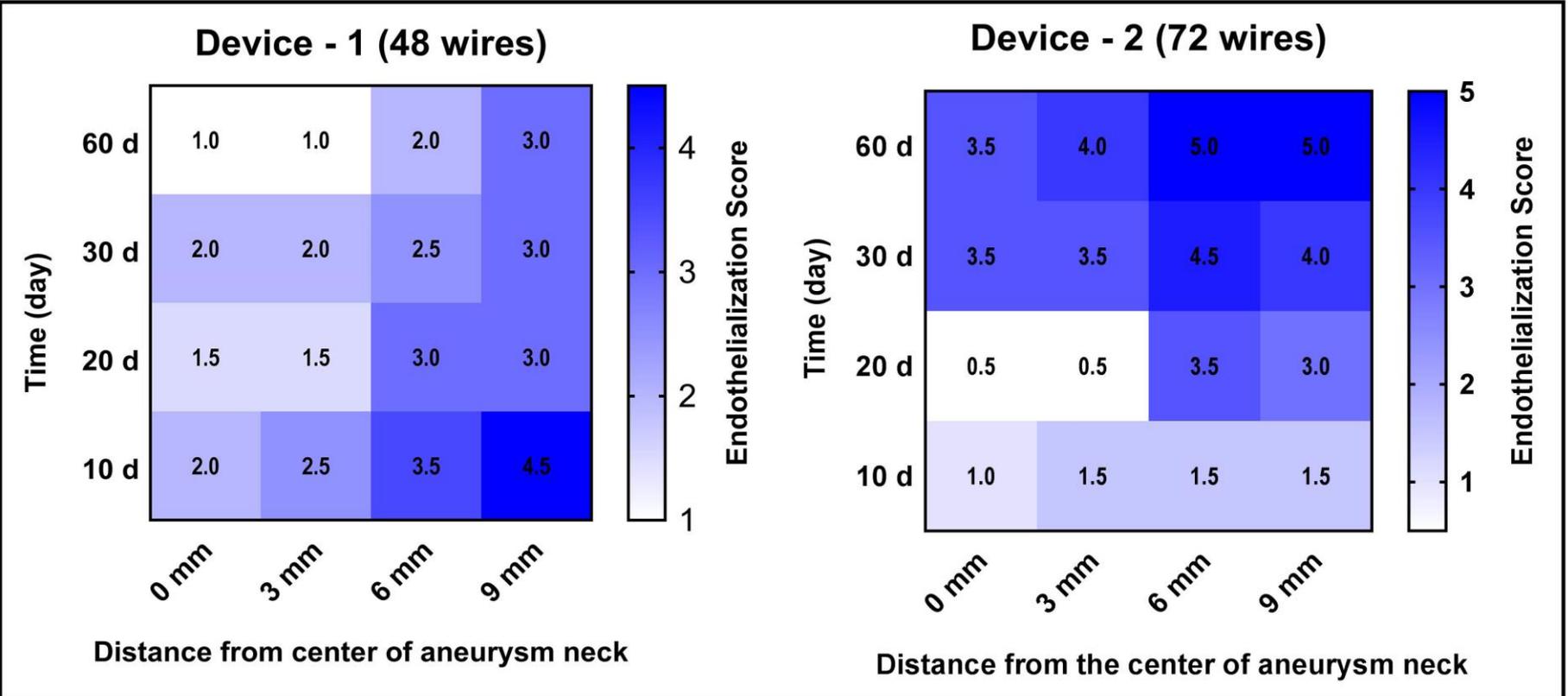
X_f → 5 mm
Y_f → 10 mm

Table 1. Scoring system for assessing the rate of flow diverter endothelialization (S-FDE)

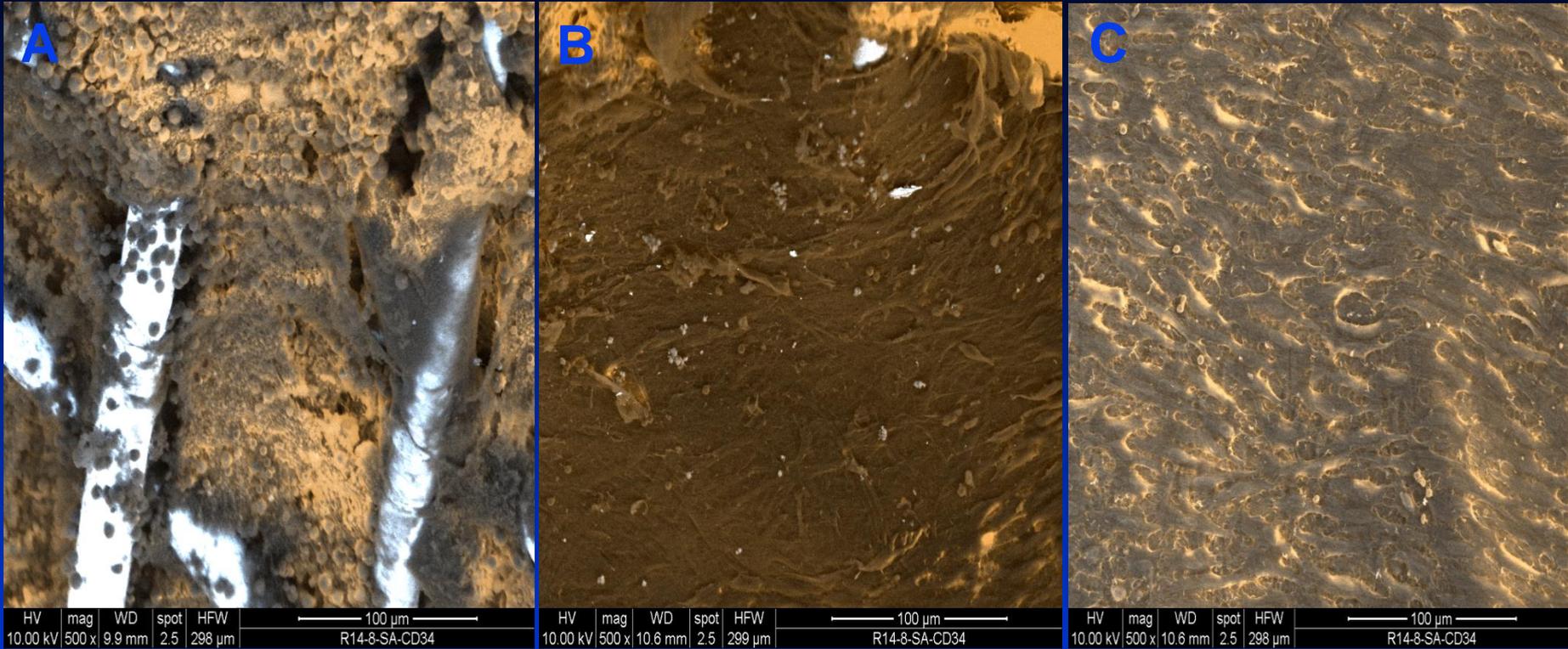
Score	Coverage of Struts	Description of Coverage
0	0%	No coverage
1	1-25%	Contains EPCs, inflammatory cells, red blood cells, proteins, and other components such as fibrin and collagen
2	26-50%	Contains EPCs, inflammatory cells, red blood cells, proteins, and other components such as fibrin and collagen for the beginning of the basement membrane
3	51-75%	Contains EPCs, inflammatory cells, red blood cells, proteins, and other components such as fibrin and collagen creating the basement membrane
4	76-99%	Contains EPCs and/or endothelial cells along with the components of the basement membrane
5	100%	Fully Endothelialized



Endothelialization



- 48-Wire (Device-1): EC scores related to location ($p=0.083$)
- 72-Wire (Device-2): EC scores are function of time ($p=0.013$)



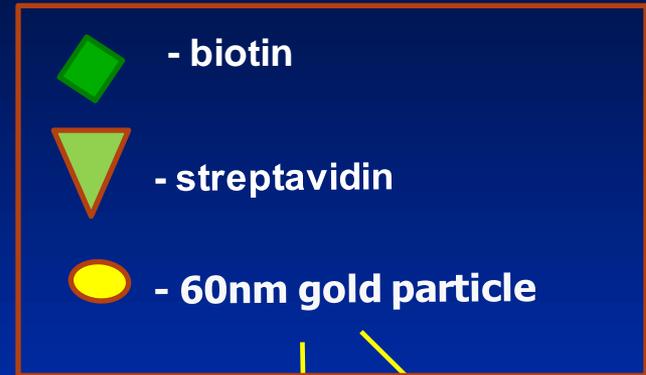
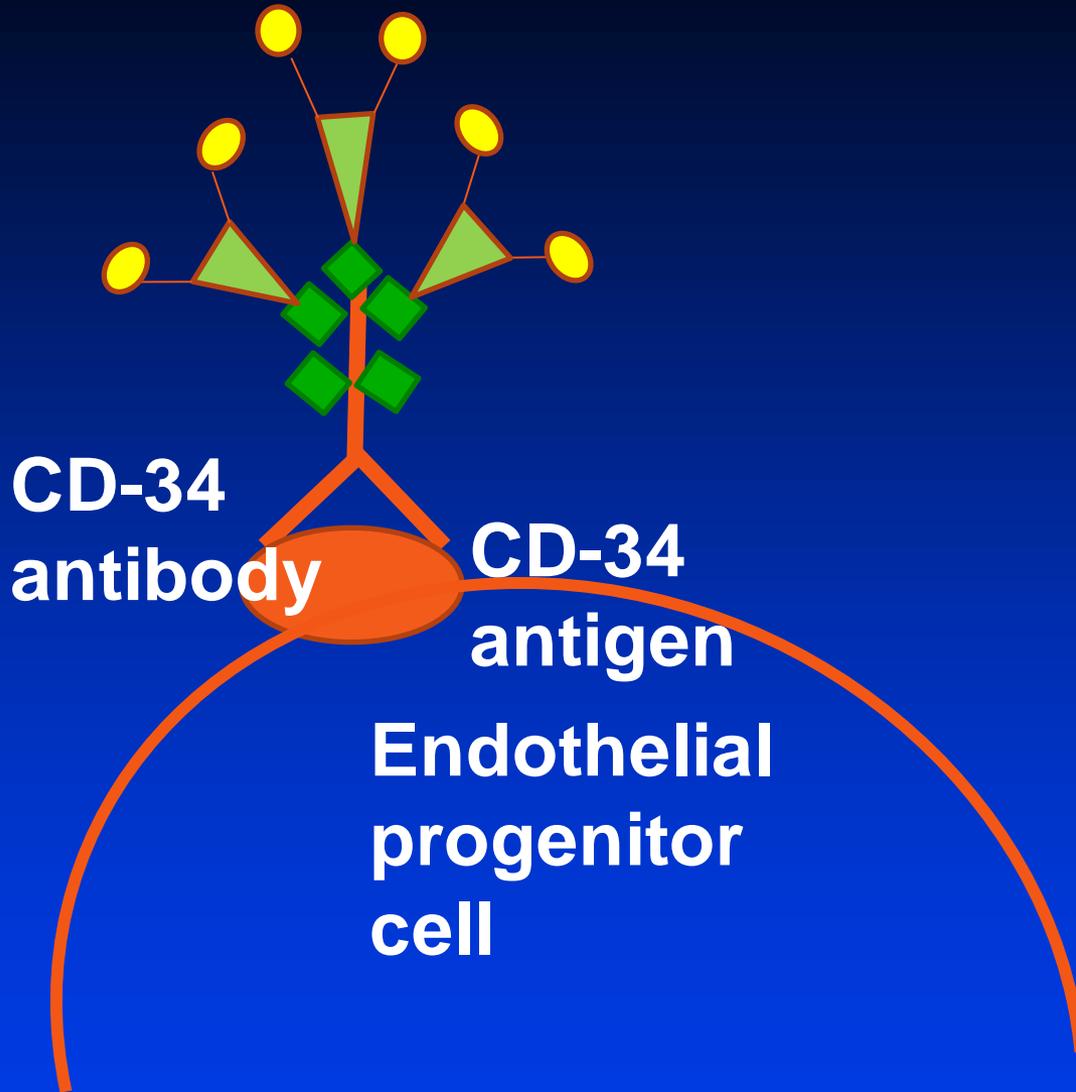
500x mag.

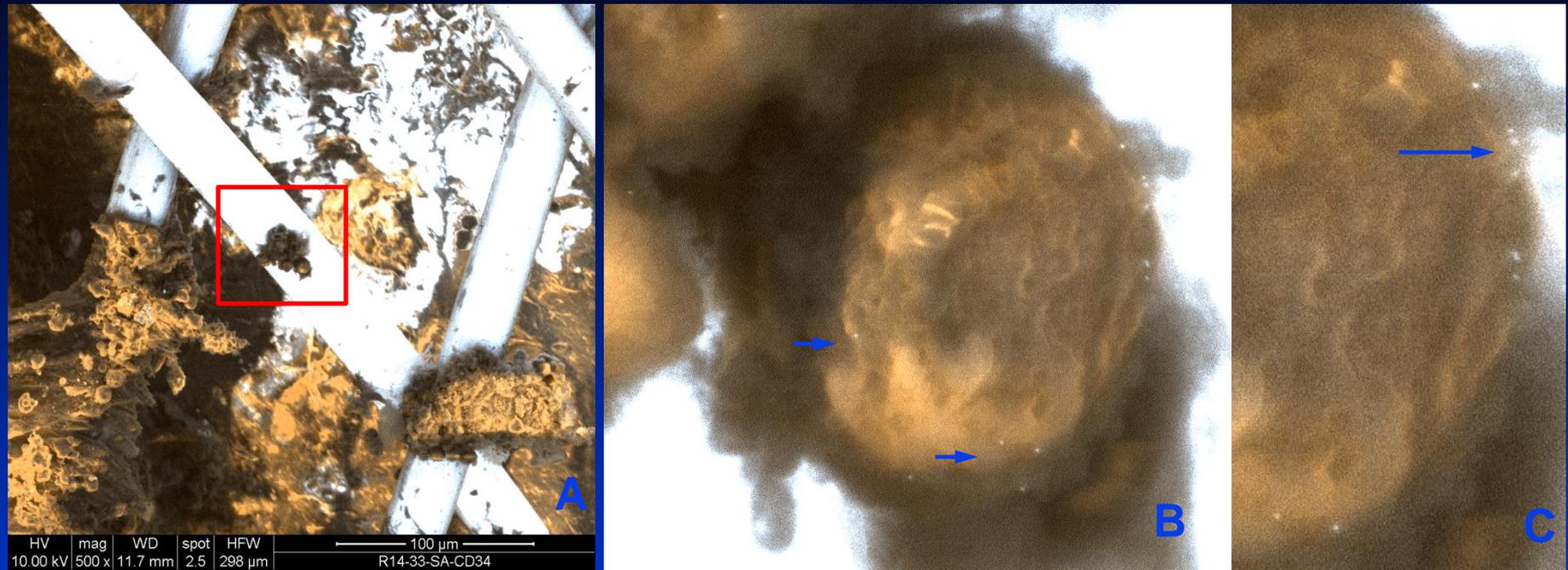
A.) center of the aneurysm neck, partial coverage of struts

B.) 2mm proximal to image A, disorganized cell network on the surface of basal membrane

C.) 5mm proximal to image A, endothelial cells are evenly distributed

Immuno-gold labeling for SEM





- A.) 500x, image of the inner surface of the NEG implant, 10 days after implantation**
- B.) 10,000x, the immuno-gold labeling on the surface of the cell (white arrows)**
- C.) manually zoom of the image B for better visualization of the gold nanoparticles**

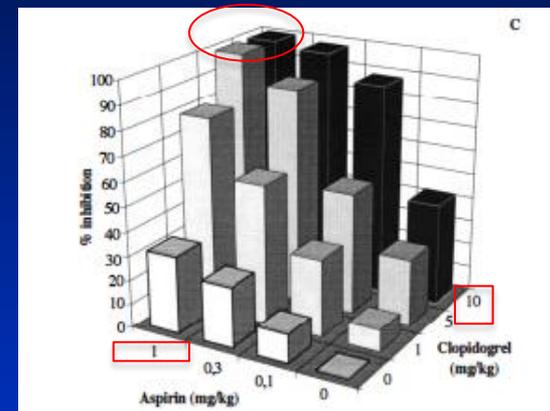
Preliminary results – anti-platelet drugs activity tests and APD (anti-platelet drug) dosing strategy

- sample collection: femoral artery
- timing: prior terminal angiography
- test: clopidogrel and aspirin activity – VerifyNow (PRU-P2Y12 Reaction Units)
- data interpretation according HUMAN studies:
 - P2Y12 Reaction Units (PRU) result of ≥ 208 were at a significantly increased risk of cardiovascular events
 - and patients with a PRU of < 95 were receiving virtually no additional protection from cardiovascular events, but at a significantly increased risk of bleeding

Thromb Haemost 1998; 80: 512-8 © 1998 Schattauer Verlag, Stuttgart

The Antiaggregating and Antithrombotic Activity of Clopidogrel Is Potentiated by Aspirin in Several Experimental Models in the Rabbit

Jean-Marc Herbert, Frédérique Dol, André Bernat, Robert Falotico¹, Alain Lalé, Pierre Savi



N=16	PRU (Clopidogrel test)	ARU (Aspirin Test)
results	102 (61-129)	652 (636-664)

N=16	In-stent stenosis	In-stent thrombosis
results	0/16 (0%)	0/16 (0%)

Flow Diversion: Summary

- Evidence: curative treatment of brain aneurysms
 - Treats diseased segment of the blood vessel
 - Endoluminal reconstruction is ideal
- Engineer construct and surface properties to promote rapid endothelialization
- Need to remove dependency on dual antiplatelet medication
- Need imaging tools developed specifically for technology to ensure proper deployment

• UMass Collaborations

- Marc Fisher, MD
- Neil Aronin, MD
- Alexei Bogdanov, PhD
- Greg Hendricks, PhD
- Guanping Gao, PhD
- Miguel Esteves, PhD
- Linda Ding, PhD
- Srinivasan Vedantham, PhD
- John Weaver, MD

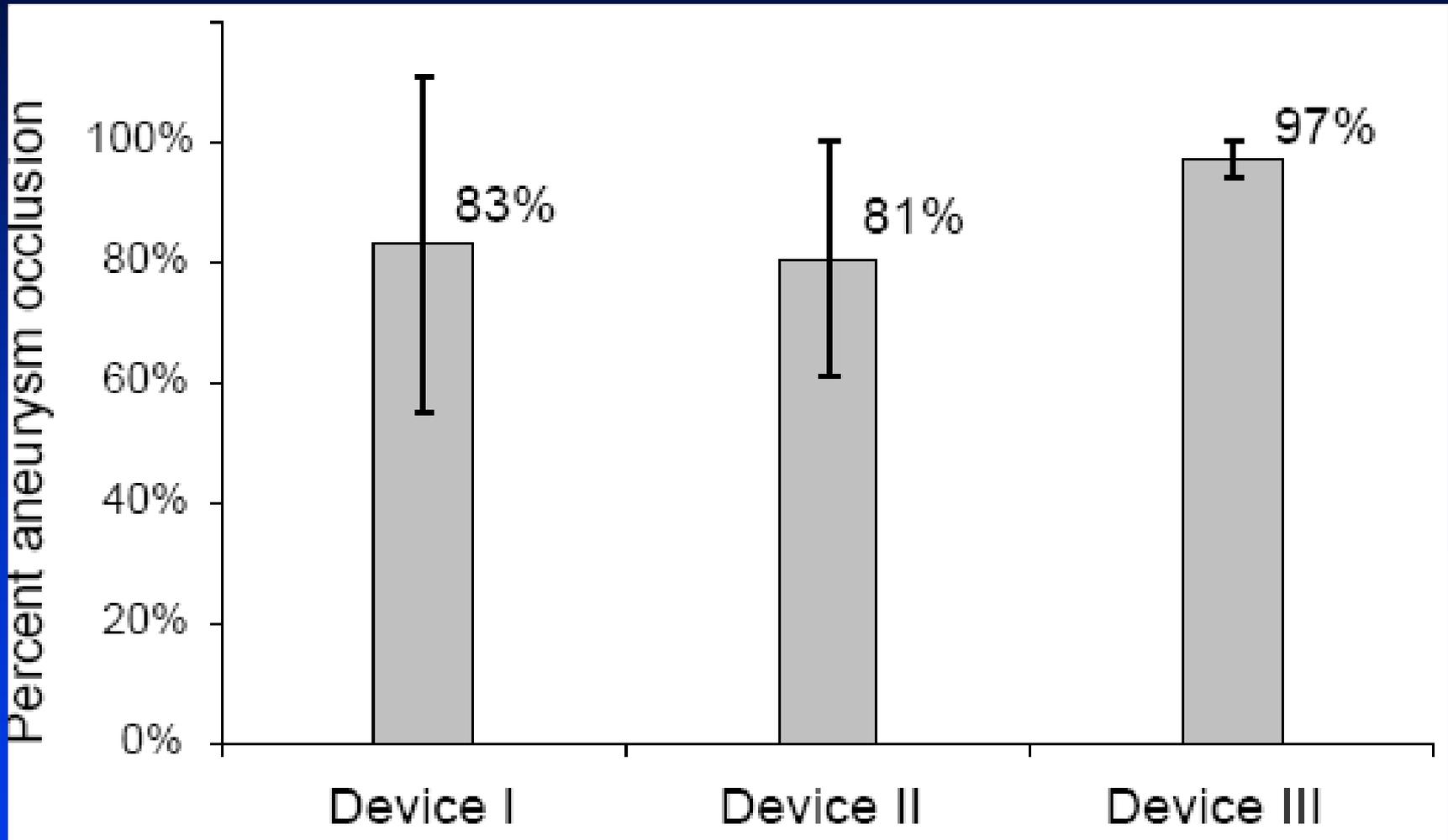
• Collaborations

- Alex Norbash, MD – BU
- Thanh Nguyen, MD - BU
- Italo Linfante, MD - Baptist
- Guilherme Dabus, MD - Baptist
- Don Ingber, PhD – Harvard
- Netanel Korin, PhD - Technion
- Johannes Boltze, MD, PhD – Fraunhofer Institute
- Raul Nogueira, MD - Emory

NECStR

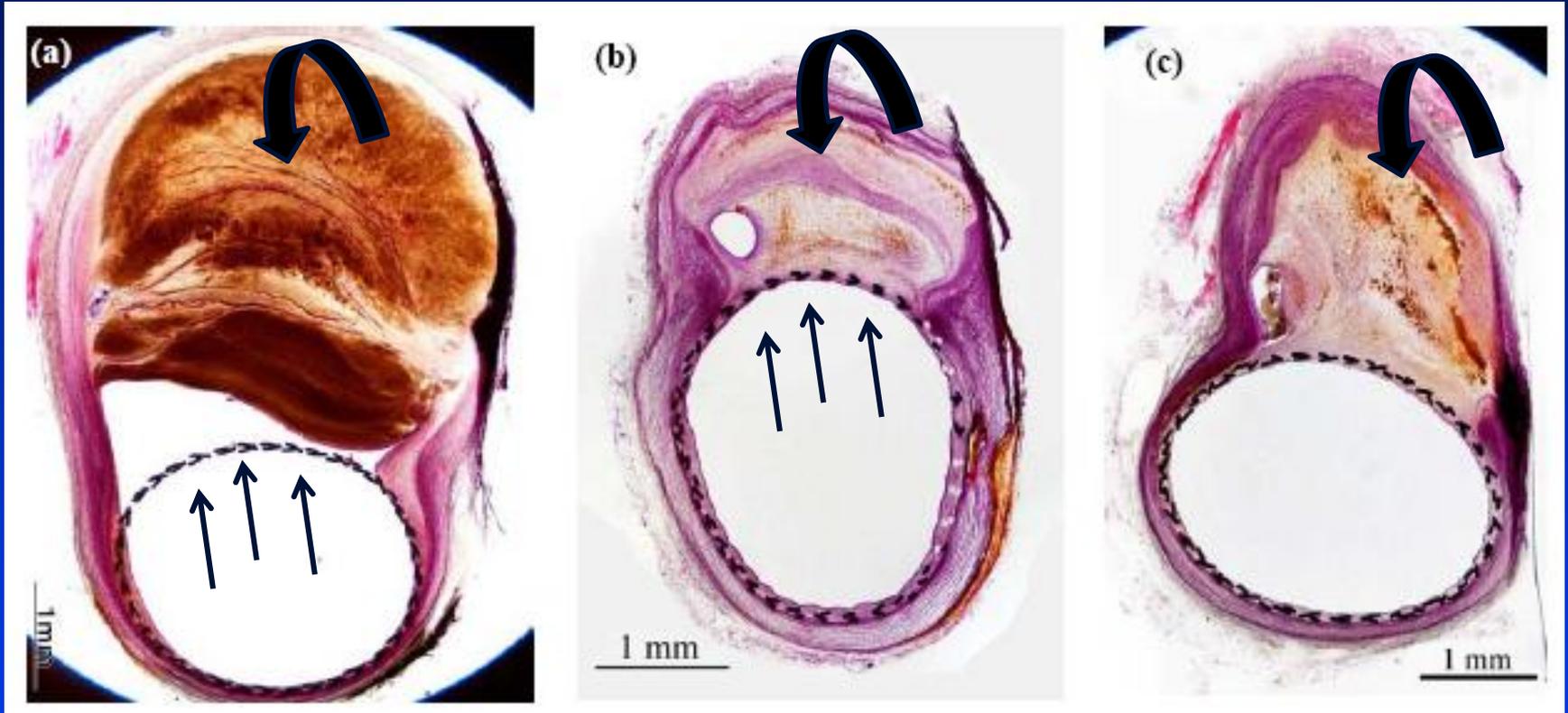
- Ajay Wakhloo, MD, PhD
- Ajit Puri, MD
- Juyu Chueh, PhD
- Miklos Marosfoi, MD
- Martijn van der Bom, PhD
- Kajo van der Marel, PhD
- Anna Kühn, MD, PhD
- Ivan Lylyk, MD
- Frédéric Clarençon, MD, PhD
- Bo Hong, MD
- Mary Howk, MS, CRC
- Thomas Flood, MD, PhD
- Erin Langan, BS
- Olivia Brooks
- Conrad Bzura, BS
- Chris Brooks, PA
- Mary Perras, NP
- Shaokuan Zheng, PhD

Mean Rate of Angiographic Aneurysm Occlusion



Histology – Progressive Occlusion – Rabbit Elastase Aneurysm Model

Amorphous clot -Organizing clot Collagen formation and Endothelialization



21 days

90 days

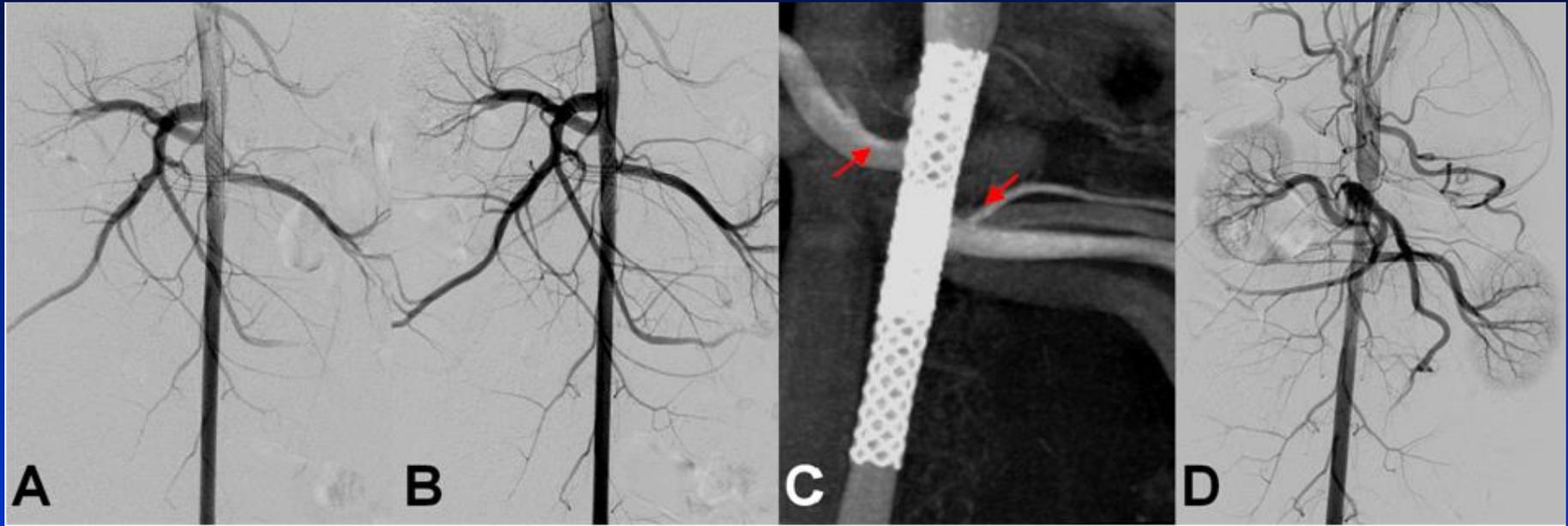
180 days

Perforators

- Large struts that cover approximately $>50\%$ of the ostium increase resistance to flow and can lead to perforator thrombosis



Perforators/ Jailed Arteries



- Model: Rabbit Aorta w/ covered Lumbar Arteries and Renal Arteries
 - Test propensity to shed emboli to kidney – both with single and double FD coverage
 - Test risk of perforator occlusion

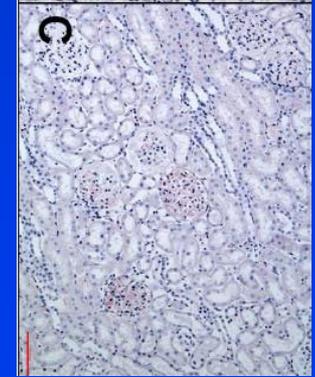
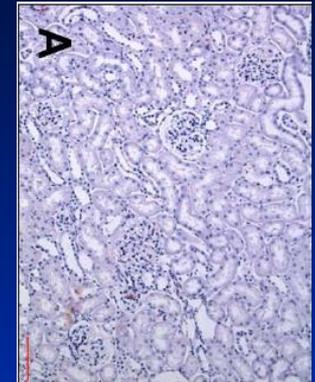
Gounis and Wakhloo, in preparation 2015

Study Design

- 45 Animals: 5 Timepoints – 7, 28, 90, 180 and 365 days
 - Per Timepoint: 6 animals for histology, 2 animals for SEM, 1 Naïve Control
 - Antiplatelet: ASA (10mg) and Clopidogrel (10mg) 4 days prior to implant, continued for 30 days
- Endpoints:
 - Vascular Response to Implants
 - Kidney histopathology
 - Perforator (lumbar arteries) patency

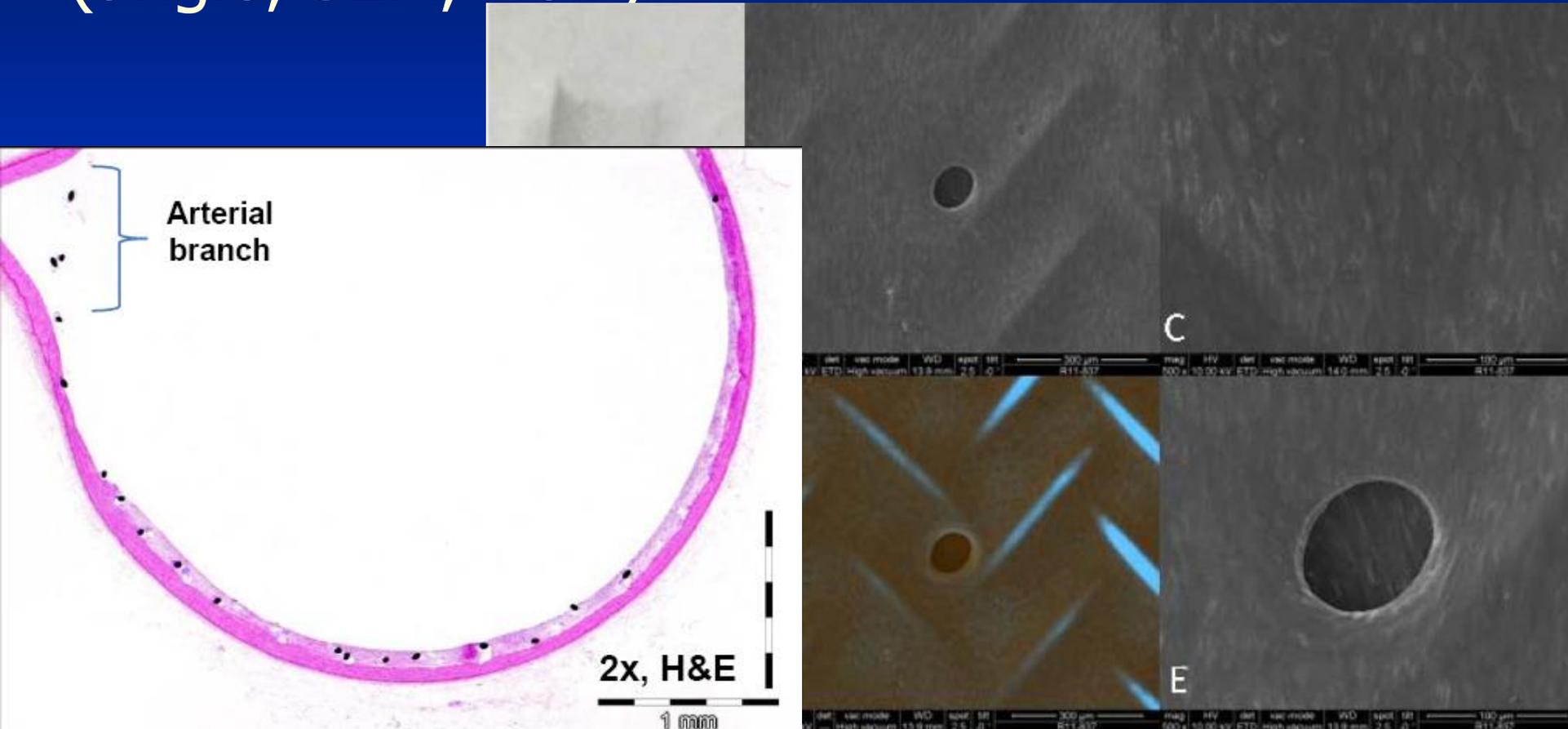
Thromboembolic Events

- Kidneys bread-loafed, 1 section each from cranial, mid and caudal aspects analyzed by light microscopy for ischemic changes
- 0 ischemic events



Perforator Patency

- All lumbar arteries remained patent (angio, SEM, H&E)



Vascular Response

- Pathology report:
 - “Histomorphometric analysis showed neointimal proliferation to be negligible at all five timepoints.”
 - “Inflammation, injury, and neointimal fibrin was overall minimal to mild in the Endograft group”
 - “showed acceptable vascular healing and produced a minimal tissue response”

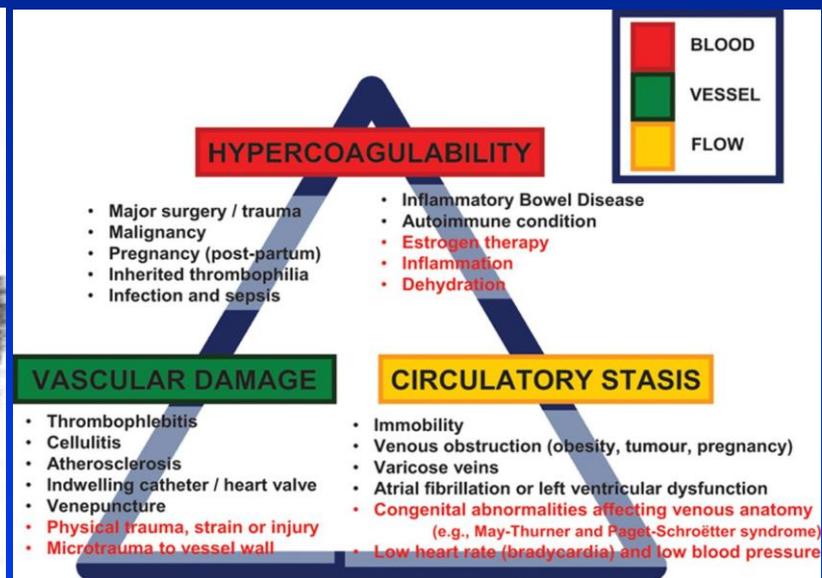
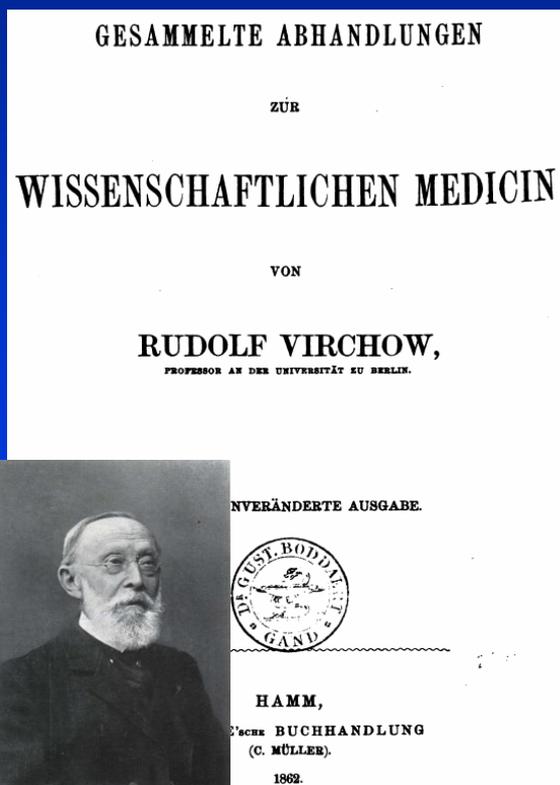


- “There was complete or nearly complete endothelialization and neointimal maturation at the 28-day time point.”

Future...

Step 1: Aneurysm Thrombosis

- Patient-Specific Hemodynamics is **ONE-THIRD** of Aneurysm Thrombosis



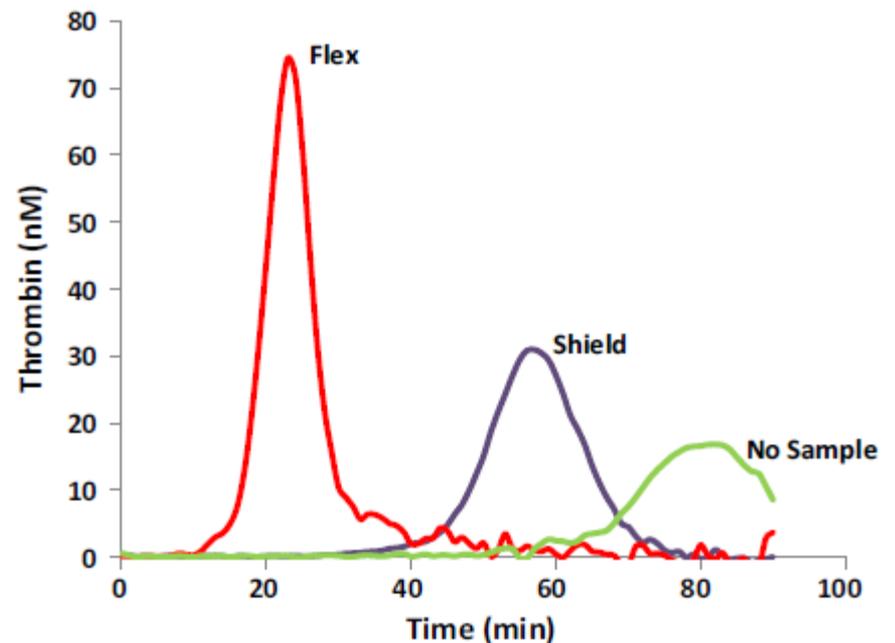
Hull and Harris, Circulation 2013

Platelets, Platelets, Platelets....

J Thromb Thrombolysis
DOI 10.1007/s11239-015-1228-0

In-vitro thrombogenicity assessment of flow diversion and aneurysm bridging devices

Gaurav Girdhar¹ · Junwei Li² · Larisa Kostousov³ · John Wainwri
Wayne L. Chandler⁴



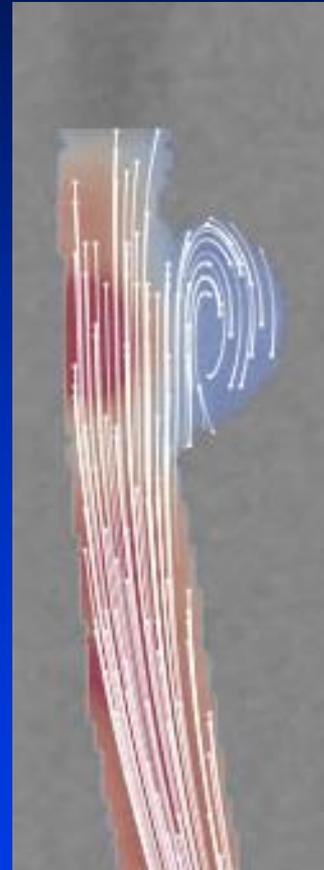
DSA-Based Intra-Aneurysmal Flow

Baseline

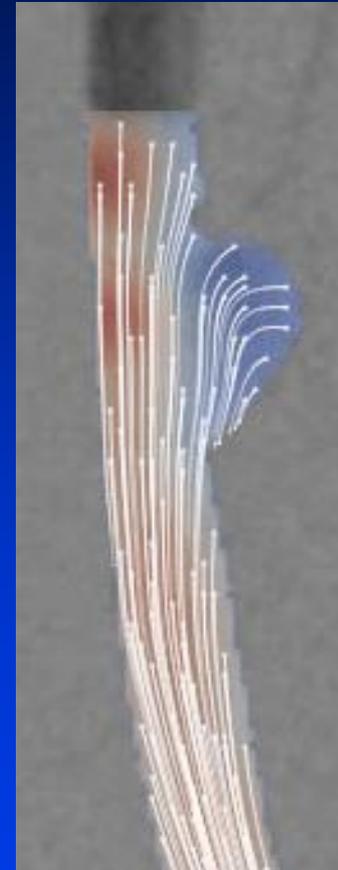
After FD implantation



DSA (60 fps)

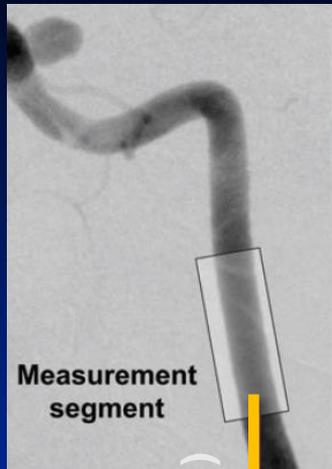


Average flow DSA (60 fps)
(projected cm/s)

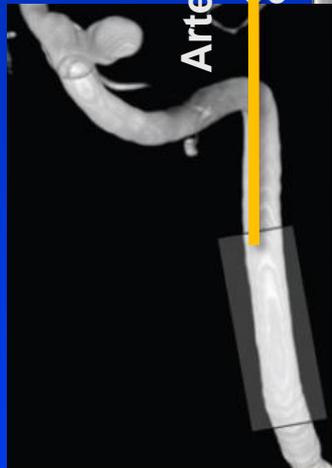


Average flow
(projected cm/s)

DSA Contrast wave map



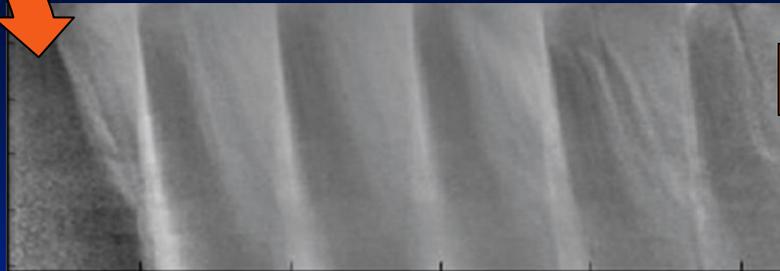
Warped 2D - 3D
Vessel Registration



3D reconstruction

Arterial axis (mm)

20
40
60
80
100

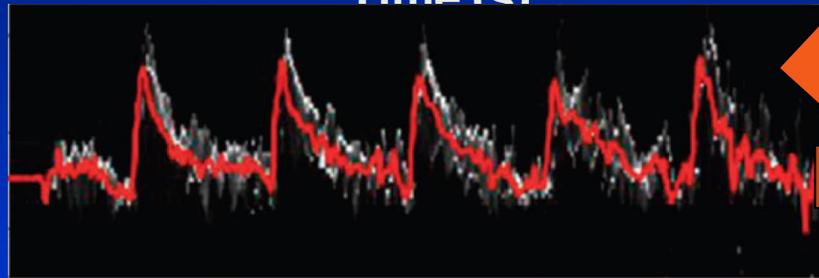


1 2 3 4 5

Time (s)

Velocities (cm/s)

40
20
0



1 2 3 4 5

Time (s)

Volume flow (ml/s)

6
4
2
0

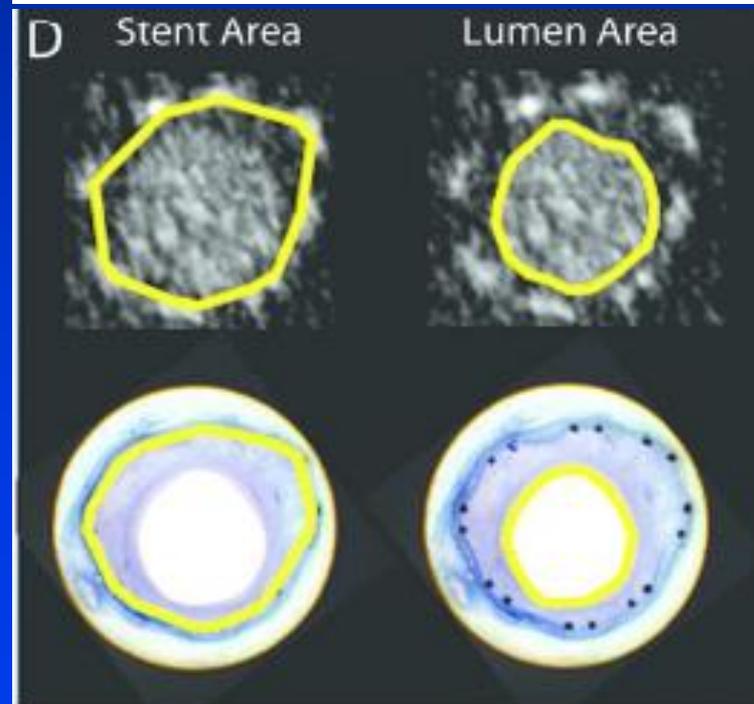
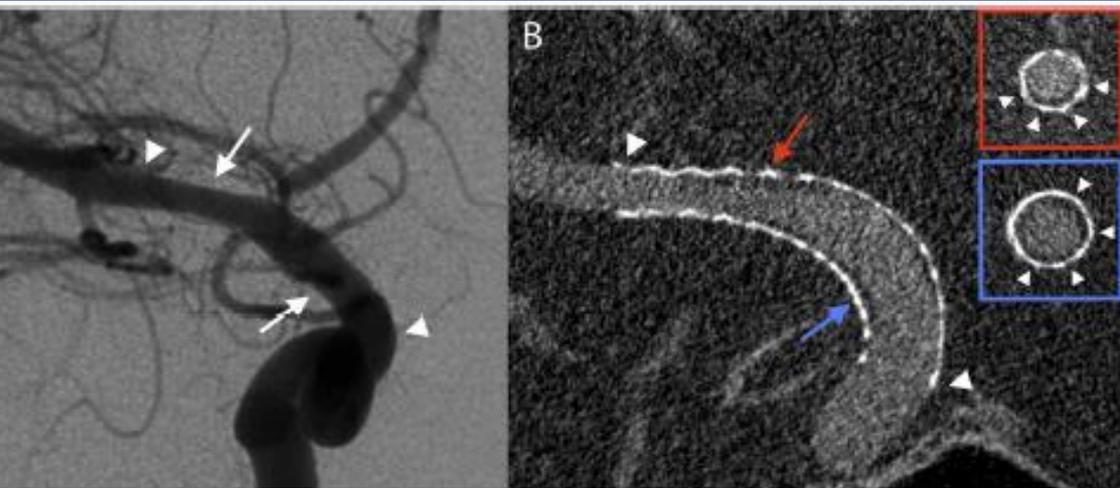
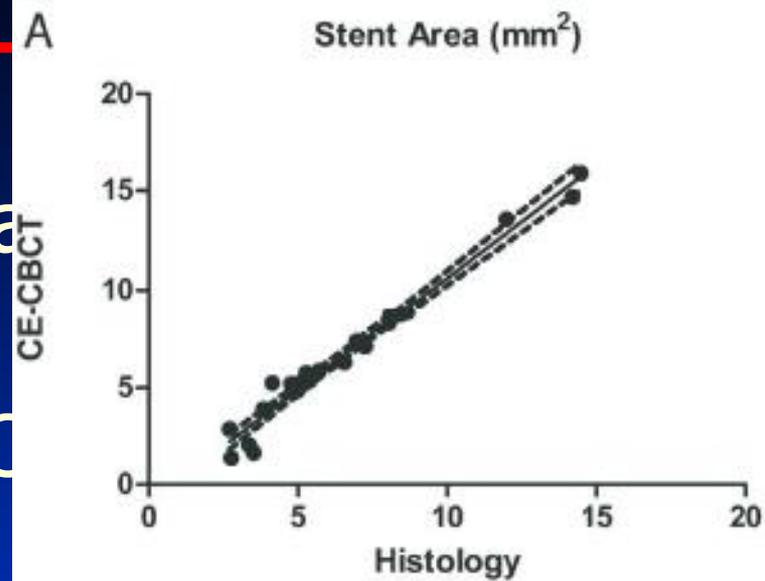


1 2 3 4 5

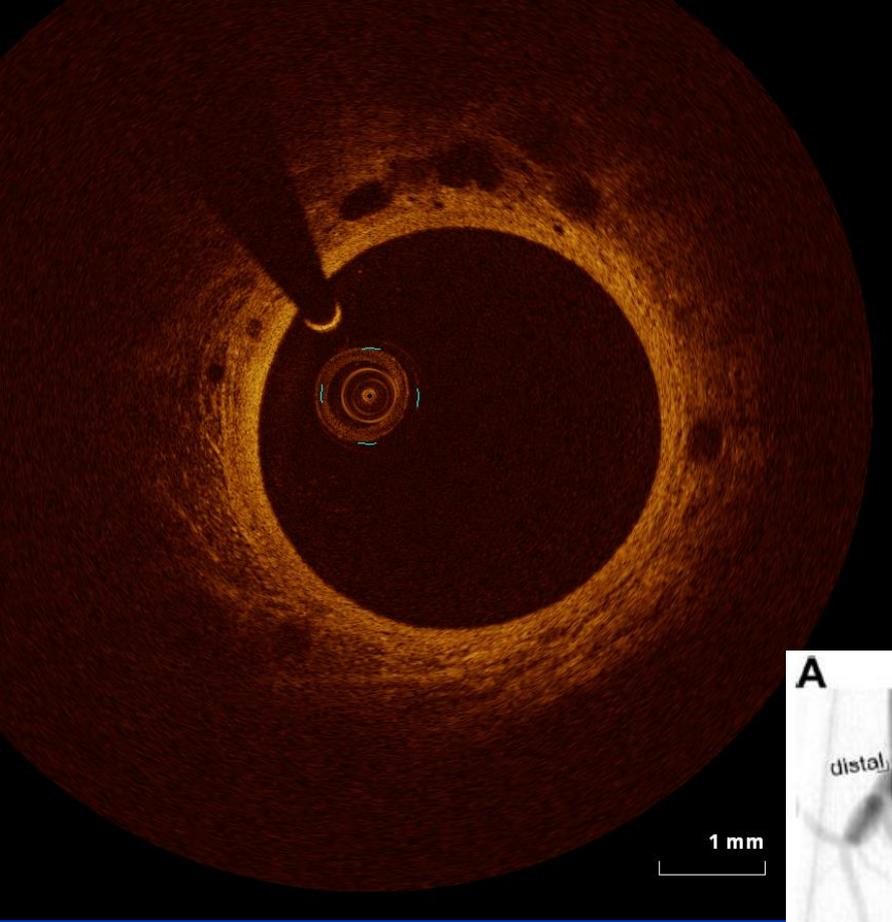
Time (s)

Apposition – Assumed!

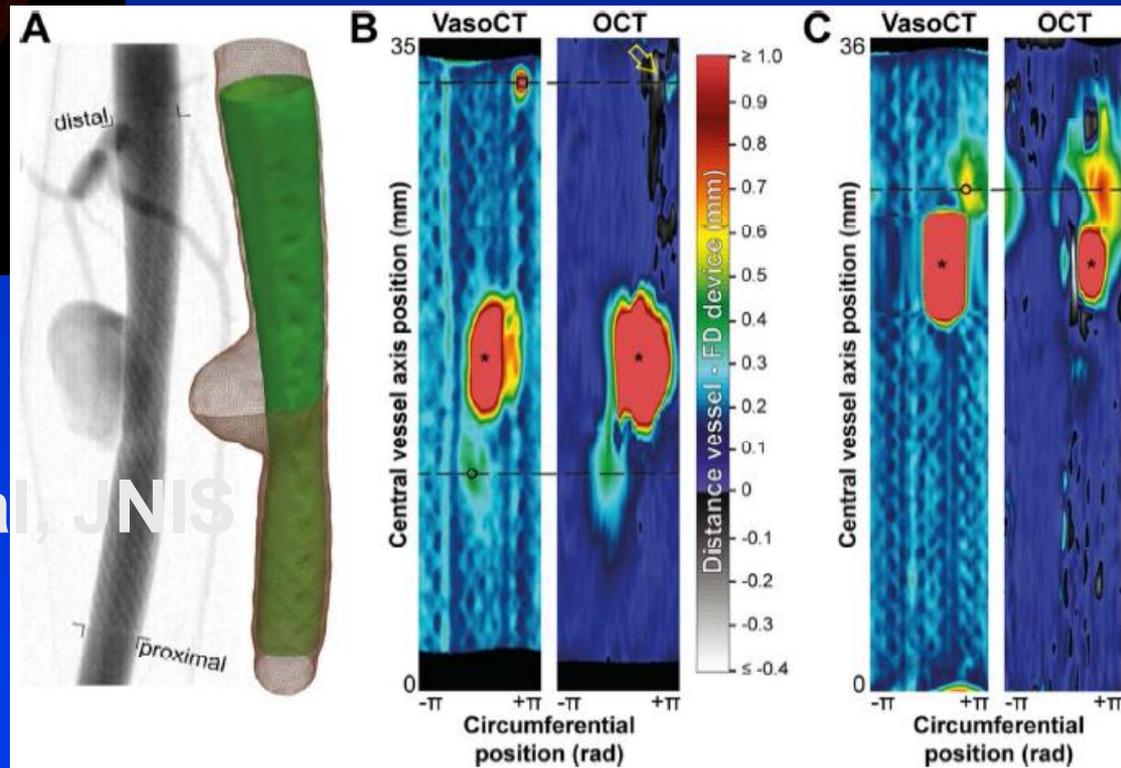
- All models assumed device apposition to vessel wall
- Non-binned, small FOV CE-CBCT



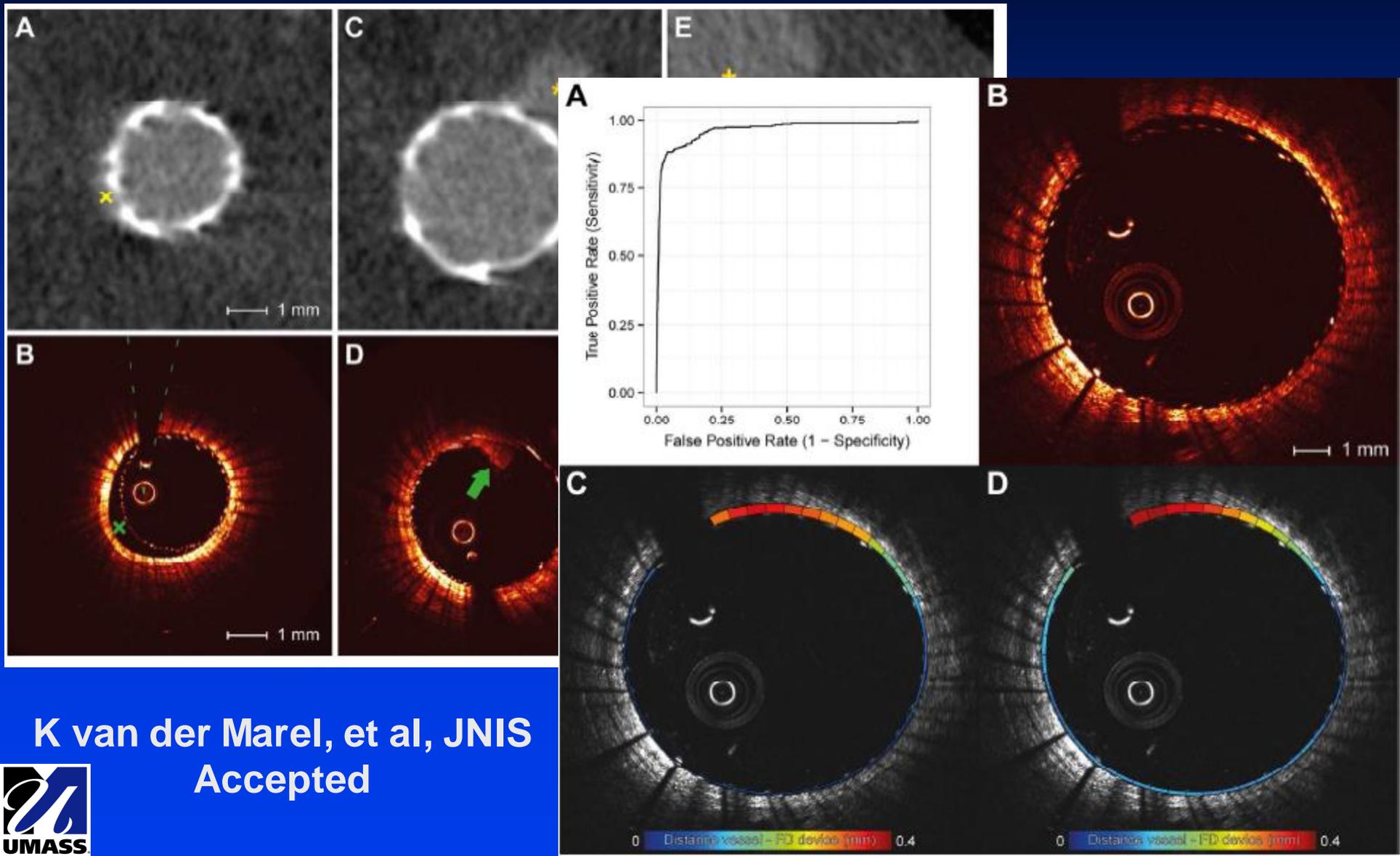
Intravascular Imaging



K van der Marel, et al, JNIS
Accepted



Intravascular Imaging



K van der Marel, et al, JNIS
Accepted

